

Correlation time diffusion coefficient brain mapping: combined effects of magnetization transfer and water micro-kinetics on T1 relaxation

H. Jara¹

¹Radiology, Boston University Medical Center, Boston, MA, United States

Purpose: To develop a T1 relaxation theory incorporating the combined effects of magnetization transfer (MT) (Ref. 1) and water micro-kinetics –i.e. translational diffusion and molecular rotations (Ref. 3-5)-- for the purpose of computing accurate **correlation time diffusion coefficient** ($D_{(CT)}$) maps of multi-pool biological tissues exhibiting magnetization transfer phenomena, such as white matter. Additionally, to test the theory's accuracy in the human brain by comparing *in vivo* and in the same subject the whole-brain distributions of the correlation time diffusion coefficient maps relative to those obtained with a standard **pulsed-field-gradient** (PFG) diffusion MRI technique: i.e. by comparing the same-subject whole-brain histograms of ($D_{(CT)}$) vs. ($D_{(PFG)}$).

Theory: Two contributions to the observed T1 relaxation rate of ¹H-proton magnetization in structurally complex aqueous biological tissue are identified. First a micro-kinetics contribution stems from translational and rotational motions of the solvent water molecules and second, a T1 contribution stems from exchange of ¹H-protons between the mobile solvent water pool and the restricted pool, specifically:

$$\left[\frac{1}{T_1} \right]_{(obs)} = \left[\frac{1}{T_1} \right]_{(solvent)} + \left[\frac{1}{T_1} \right]_{(exchange)} \quad [Eq. 1]$$

A $D_{(CT)}$ theory and associated image processing technique for the solvent water was reported earlier (Ref. 5), showing excellent quantitative accuracy for tissues devoid of magnetization transfer effects. We propose here the following model for T1 relaxation caused by MT effects:

$$\left[\frac{1}{T_1} \right]_{(MT)} = c \left(\frac{PD^{(H_2O)} - PD^{(obs)}}{PD^{(obs)}} \right) \left(\left[\frac{1}{T_1} \right]_{(obs)} - \left[\frac{1}{T_1} \right]_{(rest\ pool)} \right) \quad [Eq. 2]$$

Accordingly, the magnitude of MT-caused T1 relaxation rate is proportional to the difference in T1 relaxation rate of the restricted pool (Ref. 1) relative to the observed T1 relaxation rate. Furthermore, MT effects are also modulated by the tissue proton density relative to that of pure water at the same temperature.

Methods: Equations [1] and [2] were assimilated to the previously reported theory (Ref. 5). Brain images of a research subjects were acquired using a 1.5 T superconducting MR imaging system (NT-Intera Philips Medical Systems, N.A.). Mixed turbo spin echo (mix-TSE) is a multislice 2D pulse sequence that combines the principles of T1-weighting by inversion recovery and T2-weighting by multi-echo sampling into a single mixed MRI acquisition. Directly acquired images were post-processed, first with Q-MRI algorithms to generate the PD, T1, and T2 maps. PD maps were generated by reversing the T1 and T2 weightings of one of the mixed-TSE directly acquired images. A single shot spin-echo Echoplanar (SS-SE-EPI) sequence was used for PFG data acquisition. For both diffusion coefficient data sets, the brain was segmented using a dual-clustering algorithm and histograms were generated by pixel counting.

Results: Slice-matched $D_{(CT)}$ (top row) and $D_{(PFG)}$ (bottom row) axial diffusion coefficient maps at several locations are shown in Fig. 1. Nearly identical tissue appearance and contrast, particularly white-to-gray matter, are observed. Whole-brain histograms reflecting the $D_{(CT)}$ (yellow) and $D_{(PFG)}$ (red) are shown in Fig. 2. Both histograms are primarily unimodal and their spectral positions are nearly identical to within experimental error. The $D_{(CT)}$ distribution is measurably narrower than the $D_{(PFG)}$ distribution: increased broadening is probably the result of magnetic field inhomogeneities, to which SS-SE-EPI is considerably more vulnerable relative to the mixed-TSE sequence.

Conclusion: A T1 relaxation theory combining the effects of magnetization transfer and solvent water micro-kinetics has been developed and incorporated into a **correlation time diffusion coefficient** algorithm. This was used for 3D mapping the correlation time diffusion coefficient ($D_{(CT)}$) distribution of the human brain, leading to excellent quantitative agreement relative to standard **pulsed-field-gradient diffusion MRI**. It is concluded that magnetization transfer has a substantial effect on T1 relaxation for tissues containing a restricted pool of ¹H protons that exchanges magnetization-with the solvent.

References

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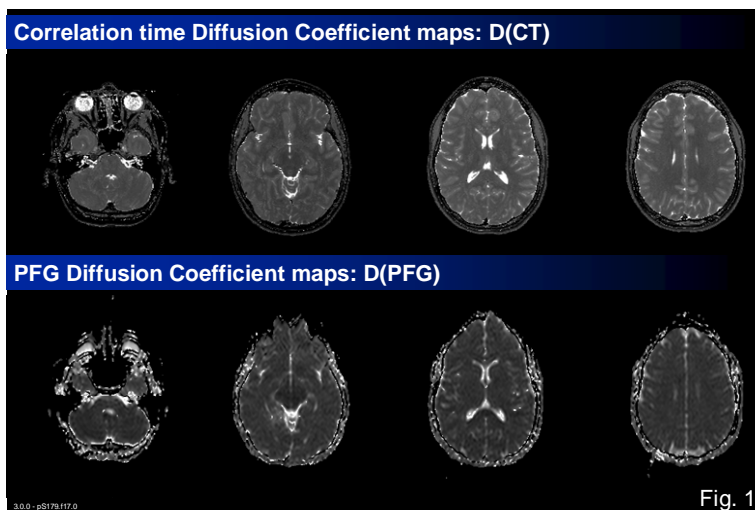


Fig. 1

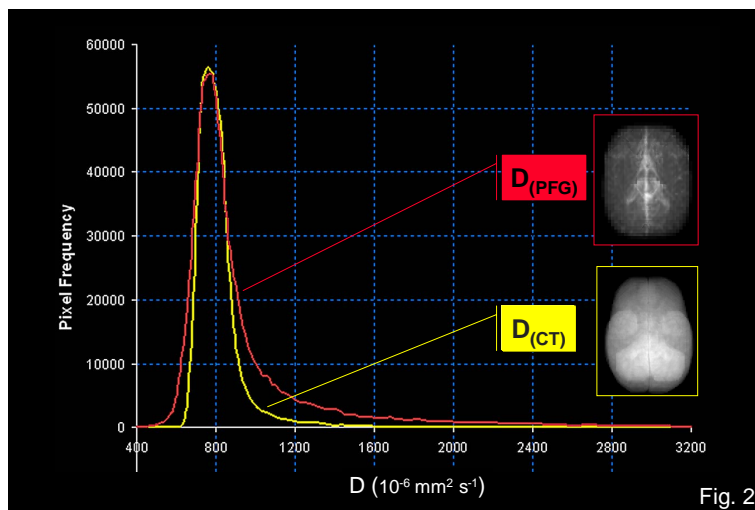


Fig. 2