

# Longitudinal tracking and quantification of T cells using *in vivo* $^{19}\text{F}$ MRI

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## Abstract

The dynamic trafficking of a specific subset of activated, antigen-specific T cells was studied *in vivo* using  $^{19}\text{F}$  MRI in an acute inflammation model for up to 21 days. The perfluoropolyether (PFPE) nanoemulsion was readily taken up by non-phagocytic T cells. T cells inoculated into a localized, acute inflammation mouse model selectively homed to the draining lymph node (DLN). The use of  $^{19}\text{F}$  MRI allows for quantification of total  $^{19}\text{F}$  signal in the DLN and apparent cell numbers. This technology allows for dynamic monitoring and quantification of cell numbers *in vivo*, without the complications of the large  $^1\text{H}$  background associated with metal-based contrast agents. These techniques can be adapted to study numerous other cell types.

## Introduction

Activated T cells are key effectors of the immune system, and can be either protective or pathogenic. Elucidating the role of T cells in an inflammatory response is of fundamental importance in a broad range of diseases, such as cancer and autoimmunity. The ability to non-invasively visualize and quantify the trafficking of inflammatory T cells is potentially a powerful diagnostic marker and can be useful in the development of new therapeutics. Previously, we developed  $^{19}\text{F}$  nanoparticles and labeling methods for activated T cells in the NOD mouse model [1]. In the present study we investigate the trafficking of activated T cells in a murine model of localized inflammation showing a reproducible trafficking of T cells to the DLN.

## Methods

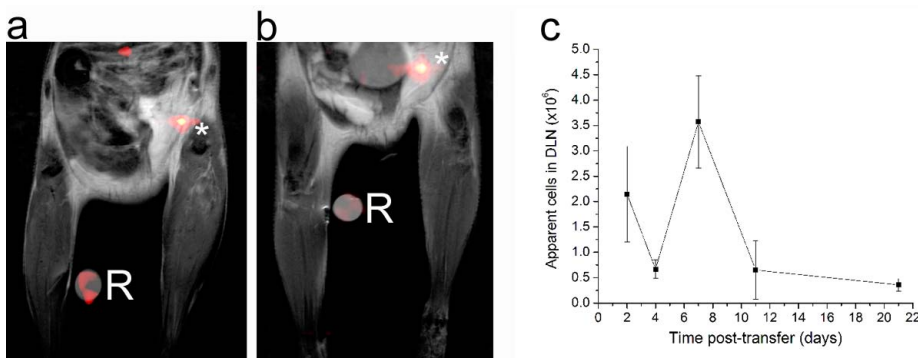
$\text{CD4}^+$  T cells ( $11 \times 10^6$ ) from DO11.10 transgenic mice [2] were purified, activated *in vitro*, labeled with PFPE nanoparticles [1], and transferred i.p. into recipient BALB/c mice ( $n=3$ ). Prior to transfer, the mice received ovalbumin in incomplete Freund's adjuvant subcutaneously near the right quadriceps. Mice were imaged longitudinally at day 2, 4, 7, 11 and 21 post-transfer. For MRI, mice were anesthetized with ketamine/xylazine by continuous infusion during the imaging session via an i.p. catheter. Mice were intubated and connected to a mechanical ventilator delivering an  $\text{O}_2/\text{NO}_2$  mixture. Respiratory-gated imaging was performed using a  $^{19}\text{F}/^1\text{H}$  volume birdcage resonator in an 11.7 T/89 mm vertical-bore micro-imaging system.  $^1\text{H}$  images were acquired with a 2DFT spin-echo sequence with  $\text{TR}/\text{TE}=1200/22$  ms and  $512 \times 256$  image points.  $^{19}\text{F}$  acquisitions used a RARE spin-echo sequence with  $\text{TR}/\text{TE}=1000/6.4$  ms and  $64 \times 32$  image points. Eight contiguous, 2 mm-thick slices were acquired for both  $^{19}\text{F}$  and  $^1\text{H}$  with a FOV of  $5 \times 2.8$  cm. The total imaging session lasted  $\sim 2$  hours. The quantity of apparent labeled cells in regions of interest was calculated directly from the *in vivo* MRI data set, an external  $^{19}\text{F}$  reference, and the  $^{19}\text{F}$  content per cell,  $F_c$ , determined from prior *in vitro*  $^{19}\text{F}$  NMR measurements of cell pellets [1].

## Results

Labeled cells were visible in the indicated inguinal lymph node, the DLN (Fig.1), and remained detectable for at least 3 weeks. Mesenteric localization was apparent only at the earlier time points (Fig. 1a). By day 11 (Fig. 1b) T cells were only visible in the DLN. Fig. 1c displays the total apparent  $^{19}\text{F}$  signal in the DLN over time. Assuming  $F_c$  is constant, this is equivalent to  $2.1 \times 10^6 \pm 9 \times 10^5$  apparent cells at day 2, dropping to  $6 \times 10^5 \pm 2 \times 10^5$  at day 4, and increasing to  $3.6 \times 10^6 \pm 9 \times 10^5$  at day 7 post-transfer. These data were validated using detailed conventional flow cytometric cell tracking, functional assays and histological studies.

## Discussion

In this study, antigen-specific PFPE labeled T cells were longitudinally tracked and quantified in an acute inflammation model. Neither T cells that were transferred without the concurrent transfer of antigen nor non-antigen specific T cells reached the DLN in appreciable numbers, highlighting the specific nature of the T cell trafficking. The inflammation model can be applied to preclinical studies of therapeutics (e.g., small molecules or recombinant proteins) that modulate T cell trafficking. The *in vivo*  $^{19}\text{F}$  platform developed here can readily be extended to other cells types including, for example, immunotherapeutics or stem cells.



**Fig. 1 Representative  $^{19}\text{F}/^1\text{H}$  coronal slices and quantification of total  $^{19}\text{F}$  signal in the DLN.**

(a and b) The MR images are an overlay of the  $^{19}\text{F}$  image (false color) and the  $^1\text{H}$  (grayscale), at day 2 (a) and day 11 (b) post-transfer. The DLN (asterisk) and external reference (R) are labeled. T cells are visible homing to the DLN. The reference (R) was used for cell number quantification. (c) The plot summarizes the quantification results for the 21 day period. Error bars represent standard deviation ( $n=3$ ).

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## References

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