## Evaluation of hyperoxic gas induced $\Delta R_1$ and $\Delta R_2^*$ as MRI biomarkers of tissue oxygenation status in human subjects

J. P. O'Connor<sup>1,2</sup>, J. H. Naish<sup>1</sup>, D. L. Buckley<sup>1</sup>, A. Jackson<sup>1</sup>, J. C. Waterton<sup>1,3</sup>, Y. Watson<sup>1</sup>, G. A. Buonaccorsi<sup>1</sup>, D. M. McGrath<sup>1</sup>, S. Cheung<sup>1</sup>, S. J. Mills<sup>1</sup>, G. C. Jayson<sup>2</sup>, and G. J. Parker

<sup>1</sup>Imaging Science & Biomedical Engineering, University of Manchester, Manchester, United Kingdom, <sup>2</sup>Medical Oncology, Christie Hospital NHS Trust, Manchester, United Kingdom, <sup>3</sup>Translational Sciences, AstraZeneca, Macclesfield, United Kingdom

**Introduction** Change in magnetic resonance signal following inhalation of hyperoxic gas may be quantified to produce biomarkers of tissue oxygenation by measuring changes in longitudinal relaxation rate  $(R_1)^{1,2}$  and effective transverse relaxation rate  $(R_2^*)^3$ . Image contrast in  $R_1$  imaging is due to the paramagnetic effect of dissolved molecular oxygen; whereas contrast in  $R_2^*$  – the blood oxygenation level dependent (BOLD) effect – reflects change in tissue levels of deoxygenated haemoglobin species. However, precise mechanisms of hyperoxia-induced  $R_1$  and  $R_2$ \* modulation are unclear. We compared the effects of 100% oxygen (O<sub>2</sub>) and carbogen (95% O<sub>2</sub>/ 5% CO<sub>2</sub>) inhalation on normal tissue  $R_1$  and  $R_2^*$  within the abdomen. It was hypothesised that the two distinct contrast mechanisms may provide complementary information concerning tissue microvasculature.

Study design Ethical approval was obtained. 10 healthy non-smoker volunteers (six female and four male; mean age 32.4 years) were recruited. All experiments took place on a Philips Intera system (Philips Medical Systems, Best, Netherlands) at 1.5 Tesla. Subjects fasted prior to scanning. They then inhaled medical air (21% oxygen) followed by 100% oxygen and then carbogen in the same order and time schedule at 15 l/min through a non re-breathing circuit with reservoir mask.

## Data acquisition

- 3D fast field echo (FFE; spoiled gradient echo) images were acquired to produce  $R_1$  maps every 76.8 s using the variable flip angle method<sup>4</sup>. (TR 3.5 ms, TE 1.  $0.9 \text{ ms}, \alpha = 2^{\circ}/8^{\circ}/17^{\circ}, 3 \text{ averages}, FOV 384 \text{ x} 384 \text{ mm}^2, \text{ matrix } 128 \text{ x} 128, 33 \text{ slices}, 3 \text{ mm slice thickness}). Data were acquired through the upper abdomen.$
- 2D multislice T2\*-weighted dual echo images were acquired over the same anatomical region to enable calculation of tissue R2\* (TR 548 ms, TE 4.6 & 18.4 2.

ms,  $a = 30^{\circ}$ , 5 averages, FOV 375 x 375 mm<sup>2</sup>, matrix 256 x 256, 25 slices, 4 mm slice thickness). Acquisition time was 327 s. 6 R1 maps and one R2\* measurement were acquired during each phase of gas inhalation. Transition phases of 8 minutes were interspersed between phases of gas inhalation to allow plateau.

Data analysis Volumes of interest (VOI) were drawn in the spleen, liver, renal cortex and subcutaneous fat. Change in  $R_1$  and  $R_2^*$  were calculated where  $\Delta R_1 =$  $(R_1(t) - R_1(air))$  and  $\Delta R_2^* = (R_2^*(t) - R_2^*(air))$ . Difference in both  $R_1$  and  $R_2^*$  across the group were evaluated using paired samples t-tests. Organ specific  $\Delta R_1$  and  $\Delta R_2^*$  were compared for each subject using Spearman's non-parametric test.

**<u>Results</u>** Mean tissue  $R_1(air)$  and  $R_2^*(air)$  were consistent with previous studies<sup>1</sup>. Significant increase in  $R_1$  was observed in all organs following inhalation of  $O_2$  and also in the spleen, liver and renal cortex when breathing carbogen (Figure 1A). In the spleen, magnitude of  $\Delta R_I$  from baseline was less when breathing carbogen than when breathing oxygen. In the liver, magnitude of  $\Delta R_I$  was increased on carbogen.  $\Delta R_1$  in the renal cortex showed no significant difference between O2 and carbogen.

In contrast, no significant  $\Delta R_2^*$  was seen for any organs when breathing 100 % oxygen. When subjects inhaled carbogen, group mean  $R_2^*$  was significantly increased in the spleen (p < 0.001), liver (p = 0.001), renal cortex (p = 0.001) and subcutaneous fat (p =0.011) (Figure 1B). Changes in  $R_1$  and  $R_2^*$  are summarised in Table 1. Subject-by-subject  $\Delta R_1$  and  $\Delta R_2^*$  did not correlate for any organ VOI during either O<sub>2</sub> or carbogen inhalation (Figure 2).

25

20

15

10

5

-5

-10

 $\Delta R_{2}^{*}$ 

-0.05

-0.1





		$R_I$ data					$R_2^*$ data				
<b>Table 1</b> Mean group $\Delta R_1$ and $\Delta R_2^*$ when switching from breathing medical air to 100 % oxygen (denoted air versus oxygen) and from baseline to inhalation of carbogen gas (denoted air versus			air versus oxygen		air versus carbogen			air versus oxygen		air versus carbogen	
	VOI	Ν	$\Delta R_{I} (s^{-1})$	p value	$\Delta R_{I} (s^{-1})$	p value	Ν	$\Delta R_2^* (s^{-1})$	p value	$\Delta R_2^*  (\text{s}^{-1})$	p value
	Spleen	9	0.157	< 0.001	0.095	< 0.001	9	-0.750	0.381	12.7	< 0.001
	Liver	10	0.045	0.002	0.084	0.001	10	-0.096	0.933	10.0	0.001
	Fat	9	0.068	< 0.001	0.095	0.08	8	-0.685	0.453	2.46	0.011
carbogen).	Renal	6	0.073	0.005	0.059	0.008	10	-1.20	0.229	9.88	0.001
30 ¬											

Spleen air - O2

Spleen air - CB

Liver air to O2

Liver air to CB

∧ Fat air to O2

△ Fat air to CB

RC air to O2

RC air to CB

0.3

ΔR₁

0.25

Discussion This study provides further evidence that the image contrast produced by  $R_1$  imaging with carbogen and/or  $O_2$  and  $R_2^*$  imaging with carbogen are different but complementary.  $R_1$  mapping with pure oxygen is a relatively simple, reliable technique, with small but measurable signal change. It is postulated that the image contrast induced by  $O_2$  inhalation in  $R_1$  mapping concerns oxygen delivery in arterioles, capillaries and presence in tissue fluid and is influenced by arterial flow, arterial blood volume and tissue metabolism.

A distinct mechanism of tissue contrast is provided by  $\Delta R_2^*$ . In our study,  $R_2^*$ imaging with O2 did not produce measurable signal change. However, marked but variable  $\Delta R_2^*$  was detected when carbogen was inhaled. Both techniques show promise as non-invasive biomarkers of tissue oxygenation.

Figure 2 Scatter-plot demonstrating the relationship between  $\Delta R_1$  (s<sup>-1</sup>) and  $\Delta R_2^*$  (s<sup>-1</sup>) for each tissue (spleen = squares; liver = circles; fat = triangle outline; renal cortex = grey-filled diamonds). Blue symbols denote transition from air to oxygen  $(O_2)$ ; points are scattered approximated uniformly around the x axis, indicating the lack of significant  $\Delta R_2^*$  for any tissue while breathing oxygen. Red symbols denote transition from air to carbogen (CB), where significant changes in both  $R_1$  and  $R_2^*$  were observed, but no clear relationship was demonstrated between the two parameters.

Acknowledgements This work was supported by Cancer Research UK (grants C19221/A6086 and C237/A6295). JHN and DMMcG are supported by AstraZeneca. <sup>1</sup>RA Jones et al., (2002) MRM 47: 728-35. <sup>2</sup>JP O'Connor et al., (2007) MRM 58: 490-6. <sup>3</sup>NJ Taylor et al., (2001) JMRI 14: 156-63. <sup>4</sup>A Haase (1990) MRM 13: 77-89.

0.35

0.1

٨

0.15

0.2