

An Optimised Elliptical Magnet for Deep Surface NMR Imaging

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Introduction. Unilateral NMR allows positioning of the sample on the surface of a portable measuring device and this technique has been used for MRS/MRI applications in materials science, biology, environmental science and medicine [1-7]. However, the open magnet geometry produces a magnetic field with high inhomogeneity, giving rise to reduced relaxation time T_2^* . The limitation due to the strongly inhomogeneous field has been overcome in MRS applications by using specialised RF coils and pulse sequences [5-6]. MRI applications require a better field homogeneity and increased penetration depth. Unfortunately, most of the unilateral devices present in the literature do not satisfy both these requirements [1-7].

Aims. Here we report the design of a novel elliptical unilateral magnet with improved field homogeneity and penetration along one direction.

Magnet Optimization and Testing. The magnet simulation and optimization has been performed using a field simulation program (RADIA) interfaced to Mathematica. The magnet model has an elliptical shape obtained by an iron yoke and 4 identical blocks of Neodymium Iron Boron (NdFeB), Fig. 1. The model is described by a set of 7 parameters including (see Fig.1): internal and external radii, eccentricity, thickness of the iron yoke, height of the blocks, angular separations between the NdFeB blocks along x and y axes. In view of the envisaged applications in surface sciences, the optimization had as a target a depth from the magnet surface between 7 and 10 mm a useful strip of about 12 mm along the x direction and width about 2 mm, see Fig. 2. The elliptical shape of the magnet allows to obtain a good uniformity in a relative large volume, but constrains its maximum field strength to 1240 G. The optimization was done to allow simultaneous acquisition from a number of strips at different depth from the magnet surface. This required the development of a multichannel MRI console that allows to acquire and process the signal from a maximum of 8 strips [8]. Fig. 3 shows a prototype of the magnet and mechanical rig for sample positioning. The magnet has been constructed by Vacuumschmelze GMBH (Germany). The magnet dimensions (170x108x50 mm³) are contained allowing the system to be portable, this being crucial for expected applications such as skin and frescoes analyses. The magnet is mounted on an aluminium support that permits rotation around the magnet z axis. The acquisition of the MRI signal from a number of radial strips is used to reconstruct 2D images. The magnetic field components were measured using a Gaussmeter (LPT- 141-2s Group3) equipped with a Hall Probe of sensitivity equal to 50 mG and a micrometric position rig. The magnet elliptical shape allows to extend the useful volume to a target region of 12x2x4 mm³ with a field inhomogeneity of less than 1500 ppm at a fixed z position (see Fig. 4 and 5). Of course better field homogeneity could be achieved with narrower strips.

Conclusions. We have designed and tested a novel elliptical unilateral magnet with improved field homogeneity along narrow strips, positioned at higher depth with respect to the existing devices. The addition of a x-gradient of about 1G/cm will suffice to distinguish different x positions at a given distance from the magnet surface without mixing signals at different z values. This opens the possibility for novel stratigraphic MRI using a multi-channel receiver.

[1] Blumich B. et al, *Magn Res Imag*, 1998, 16, 479-484; [2] Blumich B. et al, *Magn Res Imag*, 2005, 23, 197-201; [3] Haken R. et al, *JMR* 2000, 144, 195-199; [4] Manz et al, *JMR*, 2006, 183, 25-31; [5] Blumich B. et al, *Magn Res Eng*, 2002, 15, 255-261; [6] Casanova F. et al, *JMR*, 2004, 166, 76-81; [7] Prado P. J. et al, *JMR*, 2000, 144, 200-206. [8] Ciarrocchi et al, 1st Workshop MRI in NRW, Jülich Nov. 12-13, 2007.

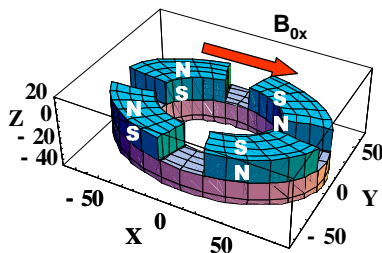


Fig. 1 Model of the magnet device.

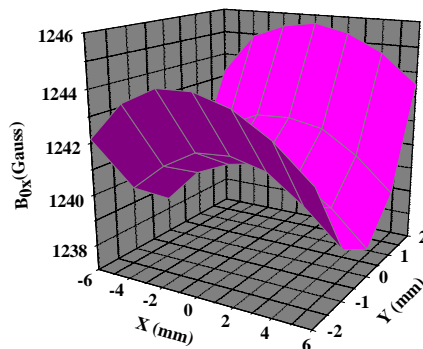


Fig. 2 The measured field B_{0x} as a function of the x and y position at a distance from the surface of $z = 7$ mm.

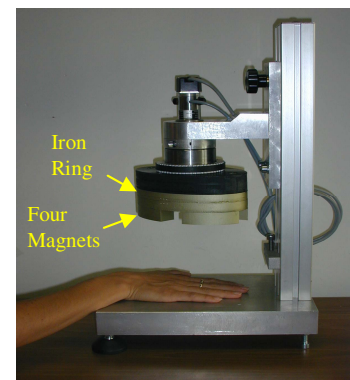


Fig. 3 Prototype of the unilateral device.

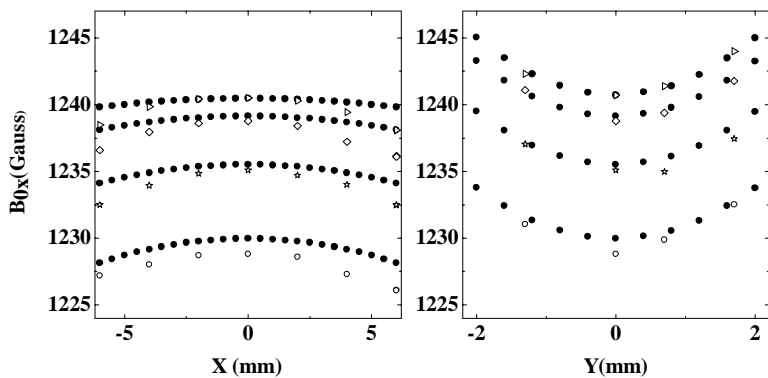


Fig. 4 The measured (open symbols) and theoretical (points) field intensity along the x (at $y = 0$) and y (at $x = 0$) directions for different distances z (in mm) from the magnet surface.

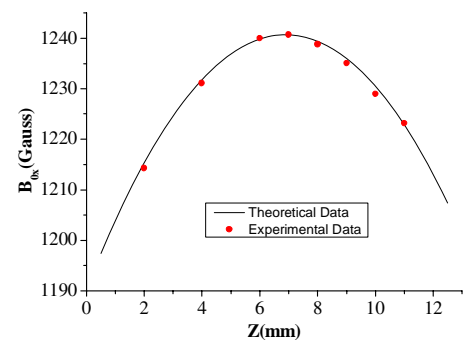


Fig. 5 The field B_{0x} as a function of the distance z from the magnet surface.