B1 Mapping Using Phase Information Created by Frequency-Modulated Pulses

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Introduction: The spatial distribution of the radiofrequency field (B1) must be assessed for a number of MRI methods, including parallel imaging. Although many techniques have been developed to map B_1 , the most straightforward and common approach is probably the double-angle method, in which the B_1 map is obtained from the ratio of two images acquired with different flip angles, α and 2α (1). A disadvantage of the double-angle method is the need to use a repetition time (TR) much greater than a longitudinal relaxation time (T_1) to obtain an accurate B_1 map. Recently, several alternative methods have been proposed to shorten TR and, thus, acquisition time. Some of them are variants of the double-angle method utilizing a driven recovery or saturation of magnetization with fast sequences (2-4). Others acquire two images from a single scan (5-6). Here, a new time-efficient method is introduced to obtain B_1 maps from multiple 2D slices. This spin-echo sequence exploits the unique properties of frequency-modulated (FM) $\pi/2$ and π pulses to create phase maps that depend monotonically on B_1 . With this method, it is not necessary for TR >> T_1 , and the $\pi/2$ and π pulses are based on the frequency- and amplitude-modulation (AM) functions of the hyperbolic secant (HS) pulse which produces excellent slice profiles (7,8).

Rationale: The basic idea of the new method originates from the observation that the magnetization phase ϕ following the application of a π HS pulse in a spin-echo sequence varies with B_1 and static field inhomogeneities (ΔB_0). In the case of a π HS pulse with the FM function sweeping from BW/2 to -BW/2 (BW = pulse bandwidth), $\phi(\Delta B_0)$ has a concave shape, with ϕ increasing as the peak of AM function (B_1^{max}) increases (Fig.1). In contrast, when the FM function sweeps from -BW/2to BW/2, $\phi(\Delta B_0)$ has a convex shape, with ϕ decreasing as B_1^{max} increases. This dependence of $\phi(\Delta B_0, B_1)$ still exists when HS pulses are used for $\pi/2$ excitation and π refocusing in 2D spin-echo imaging. According to our previous work (8), when the HS pulses are applied for both excitation and refocusing, the $\phi(\Delta B_0)$ dependence is removed if the pulse length $(T_{p,1})$ of the $\pi/2$ HS pulse is twice that $(T_{p,2})$ of the π HS pulse, i.e., $T_{p,1} = 2T_{p,2}$ (Below, subscripts of 1 and 2 indicate excitation and refocusing, respectively). Thus, ϕ depends only on B_1 , and the phase difference ($\Delta \phi$) of two images acquired using HS pulses with frequency sweeps in opposite directions can be used to calculate a B_1 map. The relationship between $\Delta \phi$ and B_1^{max} is obtained from Bloch simulation.

Method: The two images are acquired with multi-slice 2D spin-echo imaging, satisfying the condition for non-linear phase compensation across slices, i.e., $T_{p,1} = 2T_{p,2}$ (8). In the first image acquisition, HS pulses with frequency sweep from -BW/2 to BW/2 are used, and in the second acquisition, HS pulses with frequency sweep from BW/2 to -BW/2 are used. The pulse sequence diagram is shown in Fig.2 for better understanding. The two image datasets are divided to determine $\Delta \phi$. For a proper calculation of a $\Delta \phi$ map, it is recommended to isolate the object of interest and apply phase unwrapping only to the object itself, in order to avoid the phase contribution from background noise. To convert the $\Delta\phi$ map to a B_1 map, the plot of $\Delta\phi$ versus B_1^{max} needs to be obtained from Bloch simulation (Fig.3). The maximum B_1^{max} of a HS pulse was 1.34 kHz for $\pi/2$ excitation. Quadratic fitting was performed to derive an equation which specifies the relationship of $\Delta\phi$ versus B_1^{max} , that is, $\Delta\phi =$ $2.8(\gamma B_1^{\text{max}})^2 - 0.21(\gamma B_1^{\text{max}}) + 0.015$. The $\Delta \phi$ map is to be rescaled to fit the range of $\Delta \phi$ from simulation.

Experiment: For demonstration, an experiment was performed using a TEM head resonator at 4 T. The phantom consisted of a cylindrical container (diameter = 9 cm) of water with a trace amount of Gd ($T_1 \approx 1$ s). In the presence of same slice-selective gradients, $\pi/2$ and π HS pulses of the same BW (= 2.5 kHz) were used with $T_{p,1} = 8$ ms and $T_{p,2} = 4$ ms, respectively. Other parameters were: FOV = 20×20 cm², matrix = 128×128, TE/TR = 20 ms/0.5 s, acquisition time = 66 s, and slice thickness = 5 mm. In the obtained B_1 map (Fig.4), the maximum B_1 occurred in the center of the phantom, and B_1 intensity was gradually decreasing when approaching the periphery of the phantom. The maximum B_1 variation was ~31.4 %.

Conclusion: The new B_1 mapping method presented here is obtained by calculating the phase difference between two spin-echo images obtained with HS pulses having opposite frequency sweeps. Unlike the original double-angle method in which $TR >> T_1$, the new method can reduce scan time by shortening TR because of its use of phase, not signal magnitudes, and it can avoid a possible problem due to different slice profiles caused by using different flip angles (6). It can also be applied to both a volume coil and a surface coil, and 2D multi-slice B_1 map can be obtained.

References: (1) Insko EK et al, JMR 1993:82-85 (2) Stollberger R et al, MRM 1996:246-251 (3) Wang J et al, MRM 2005: 666-674 (4) Cunningham CH et al, MRM 2006:1326-1333 (5) Pan JW et al, MRM 1998:363-369 (6) Yarnykh VL, MRM 2007:192-200 (7) Park J-Y et al, MRM 2006:848-857 (8) Park J-Y et al, ISMRM 2006 Acknowledgements: This work was supported by NIH grants P41 RR08079, R01 CA92004, Keck Foundation, BTRR P41 008079, and MIND Institute. The authors thank Dr. Pierre Francois van de Moortele for insightful discussions.



Fig.1 A 3D plot showing $\phi(\Delta B_0)$ shifts in ϕ magnitude as B_1^{max} increases, where $\phi(\Delta B_0)$ was produced by a π HS pulse whose frequency sweeps from BW/2 to -BW/2 for a given B_1^{max} . sweep direction must be opposite.



(kHz) 1.3 1.2 1.1 1.0 0.9 0.8

Fig.2 Multi-slice 2D spin-echo sequence diagram. In experiment 1, HS pulses with frequency sweep from -BW/2 to BW/2 are used. In experiment 2, the frequency-

π/2 HS

Fig.3 A plot of $\Delta \phi$ versus B_1^{max} which was obtained from Bloch simulation. Quadratic fitting was performed to determine the equation which specifies the relationship of $\Delta \phi$ versus B_1^{max} .

Fig.4 The B_1 map obtained from the new B_1 mapping method. For better demonstration, the background was scaled to be a half of the maximum B_1 .