Optimization of In-phase and Opposed phase Imaging at 3T for Abdominal MRI

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Introduction

Dual gradient echo In-Phase(IP) and Opposed-Phase(OP) imaging (or Dixon's technique) is used routinely in body imaging for a broad range of clinical diagnoses, including hepatic steatosis, adenomas and renal angiomyolipomas^{1,2}. This sequence can also be used to quantify the fat content of pathology³. IP/OP imaging is based upon periodic addition (IP) or cancellation (OP) of fat and water signals due to their chemical shift. The difference of frequencies is $\Delta\omega$ =223Hz at 1.5T which results in n echo times of (2.24 + n 4.47) ms for OP, and (4.47 + n 4.47) ms for IP acquisition. At 3.0T, the difference is twice as large $\Delta \omega$ =447Hz, resulting in shorter echo times of (1.12 + n 2.24) ms for OP and (2.24 + n 2.24) ms for IP acquisition. The shorter echo spacing causes the sequence to use the technical limits of the gradient and RFpower system of the scanner at 3T. The purpose of this study was to optimize a IP/OP gradient echo protocol by varying bandwidth (BW) and echo asymmetry (EA) in order to achieve desired echo times and to assess the effects on T1-weighted image contrast and fat quantification potential.

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Table #1					
TE[1]	TE[2]	BW[1]	BW [2]	EA[1]	EA[2]
(ms)	(ms)	(Hz/px)	(Hx/px)		
2.46(I)	3.69(O)	750	780	.60	.40
1.23(O)	4.92(I)	750	750	.21	.50
3.69(O)	4.92(I)	780	780	.59	.40
1.58(O)	2.93(I)	1090	930	.46	.50

Figure1 Comparision of Opposed Phase Echoes for Optimized Pairs 1.0 100% Water 1400 1200 0.5 Index = (SI_p-SI_{op})/SI 100% Fat 100% Water 1000 Signal(AU) 0.0 800 600 -0.5 400 TE 1.23 (BW750/EA.21) 5 -1.0 TE 1.58 (BW1090/EA.46) 200 TE 3.69 (IP4.92)(BW780/EA.59) TE 1.58(O) / 2.93(I) TE 3.69(O) / 4.92(I) 0 -1.5 10 0 -5 10 5 Slice Position



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A phantom filled with vegetable oil (fat) and distilled water was imaged using a spoiled gradient echo sequence (FLASH) with FOV 300x225 mm, matrix=154x256, TR 182 ms, iPAT = 2 and flip angle 90° . Based on the signal intensity equation for FLASH, the largest contrast C= SI_{diff} / SI_{average} of a variety of tissues with published T1

> implementation due to time constraints imposed by the RF pulse and spatial encoding gradients. Hence, the closest approximation 1.58(OP)/2.93(IP) was acquired. 6 subjects (2 with fatty liver) were scanned with the same dual gradient echo protocol. For phantom and human studies, comparison of the echo pairs were quantified using a signal intensity (SI) index = $(S_{IP} - S_{OP})/S_{IP}$ and optimal contrast. Results

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Phantom results show the greatest range of signal and with TE 1.23(O) (Fig 1). As expected, exact OP times result in

Table #2In Vivo Results		In-phase Contrast		
Protocols	Mean SI Index for Fatty Liver Cases (n=2)	Liver/Spleen Contrast (n=6)	Spleen/Pancreas Contrast (n=6)	
2.46(I) / 3.69(O)	.67	.053	.134	
1.23(O) / 4.92(I)	.55	061	.085	
3.69(O) / 4.92(I)	.53	064	.058	
1.58(O) / 2.93(I)	.34	088	.074	

ellation of signal compared to partial opposed phase, TE 1.58(O) (Fig 1). Of the optimal TEs compared, the echo pair 2.46ms (I) / 3.69ms (O) shows slightly higher relative signal difference compared to other optimal pairs (Fig 2). Comparison of IP conditions show highest liver/spleen contrast and spleen/pancreas contrast for TE=2.46ms (Table2). Contrast is reduced or inverted at later echoes due T2* decay of tissues of interest.

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Discussion

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Slice Position

To achieve optimal signal difference it is essential that exact in-phase and opposed-phase times are acquired. Conventionally, the OP echo is acquired before the IP to ensure that signal loss in the OP image is caused by

intravoxel fat and water instead of T2* decay. Acquiring the IP echo before the OP, at 2.46 ms (I) / 3.69 ms (O), could be a viable option as long as the minimum difference between the echoes is maintained. Our results suggest that this pair can also enhance the identification of fatty liver. In the future, modified sequences that

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