

Improving Myocardial Perfusion Imaging with B₀- and B₁-Insensitive Saturation RF Pulse at 3T

W. Sun¹, Y. He², G. Cao³, T. Foo⁴, and Z. Zhang²

¹GE Healthcare, Waukesha, WI, United States, ²Beijing Anzhen Hospital, Beijing, China, People's Republic of, ³GE Healthcare China, China, People's Republic of, ⁴GE Global Research Center, Niskayuna, NY, United States

Introduction: First-pass myocardial perfusion MRI is a potential noninvasive method for assessing the severity of coronary artery disease [1]. The accuracy of assessing myocardial perfusion with MRI mainly depends on contrast-to-noise (C/N) and peak contrast enhancement (pCE). Recent study showed that the longer pre-contrast myocardial T₁ at 3T leads to more pCE and C/N than at 1.5T [2]. However, the incomplete saturation of magnetization due to the static magnetic field (B₀) and radio-frequency field (B₁) inhomogeneities becomes more problematic on 3T which hence impair the robustness of 3T perfusion imaging. The former study demonstrated that the BIR-4 RF pulse [3] can improve the saturation performance at 1.5T [4]. The purpose of this study was to compare the BIR-4 pulse with the typically used HARD RF pulse on 3T and evaluate the perfusion sequence on human subjects.

Methods: A gradient echo sequence with cardiac gating and a nonselective saturation RF preparation was employed for the first-pass imaging. The imaging parameters were field of view = 370x296 mm², acquisition matrix = 128x96, in-plane resolution = 2.89x3.08 mm², slice thickness = 8mm, TE/TR = 1.3/3.3ms, flip angle = 10°, bandwidth = 976.6 Hz/pixel. Two saturation pulses were implemented: nonselective HARD 90° and nonselective BIR-4 90°. The pulse durations for HARD 90° and BIR-4 90° were 1ms and 8ms respectively. A proton density weighted (PDW) image without saturation RF was also acquired as a reference. The inhomogeneities caused by the transmit RF, dielectric and receive coil can be corrected using the PDW image. The experiments were performed on a 3T Signa Excite HD scanner (GE Healthcare, Milwaukee, USA) with an 8-channel torso phased array RF coil 7 human subjects (4 volunteers and 3 patients) were imaged with 3 short-axis views (apical, mid-ventricular, basal) and 2 long-axis views (2-Chamber, 4-Chamber). A single dose (0.1mmol/kg) contrast was injected at 5mL/s for the three patients. The myocardial delay enhancement (MDE) study was also performed at the same anatomic locations. The residual magnetization (M_R) was calculated by S_{SAT}/S_{PDW}. Two ROIs were selected in apical and basal myocardium respectively from the 4-Chamber plane image as Fig. 1. shows. The ratio of S_{ROI1}/S_{ROI2}, which reflects the saturation uniformity, were calculated and corrected using the PDW image.

Results: Fig. 1 shows example images of M_R in a 4-chamber view heart. In all seven human subjects, the mean M_R was significantly different between the BIR-4 and HARD RF pulses (M_{R,HARD}=0.21±0.06; M_{R,BIR-4}=0.14±0.03; p<0.001). Besides this, the mean ratio of S_{ROI1}/S_{ROI2} was also significantly different (S_{1,HARD}/S_{2,HARD}=1.57±0.05; S_{1,BIR-4}/S_{2,BIR-4}=1.06±0.05; p<0.001). The perfusion imaging using BIR-4 saturation successfully identified perfusion defect in 2 patients which were verified by MDE. Fig. 2 shows the first-pass myocardial perfusion images (A-D) and the corresponding MDE image (E) of one case.

Conclusion: This study demonstrates that the saturation performance of BIR-4 RF pulse is much better than HARD RF pulse when there are B₀ and B₁ inhomogeneities. BIR-4 saturation pulse together with gradient echo acquisition sequence can provide satisfactory image quality for perfusion study at 3T and is feasible to detect ischemia heart disease.

Reference: 1. Wilke, N et al. Radiology 1997; 204:373-84. 2. M. Jerosch-Herold et al. Proc. Intl. Soc. Mag. Reson. Med. 13 (2005): 1623. 3. Staewen, RS et al. Investigative Radiology 1990; 25:559-67. 4. D. Kim et al. Proc. Intl. Soc. Mag. Reson. Med. 13 (2005): 520.

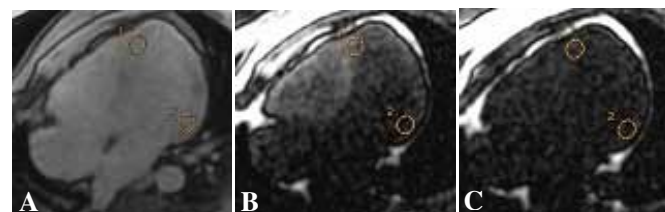
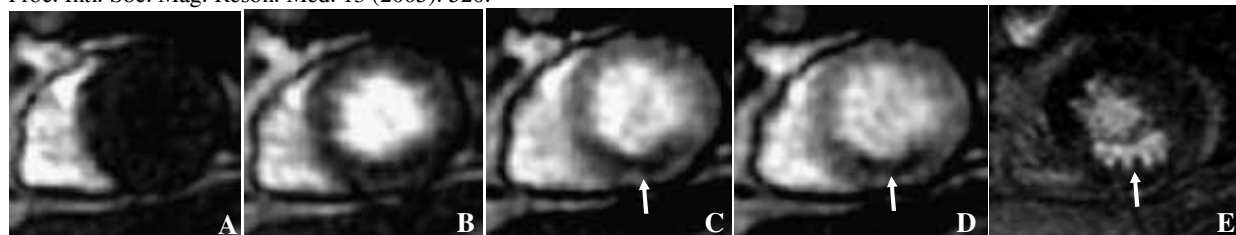


Fig. 1. Example images of residual magnetization in a heart of the 4-chamber view, comparing the performance of the two saturation pulses: (a) PDW, (b) HARD 90°, (c) BIR-4 90. (b) and (c) are displayed with same WW and WL.

Fig. 2. First-pass myocardial perfusion with BIR-4 90° saturation RF of one patient. (A)-(D) are the perfusion images from different phases after the contrast injection. (E) is the corresponding image from myocardial delay enhancement study.