

Evaluation of 3D-EPI PULSAR with and without Background Suppression Inversion Recovery Pulse

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Introduction

Modification of the recently introduced PULSAR technique [1] by use of a non-selective inversion pulse along with 3D-Turbo Field EPI (TFEPI) acquisition, labeled IR-3D-PULSAR (for CSF suppressed Inversion Recovery), is described here. Single-shot 3D acquisition schemes eliminate slice dependent variation of the perfusion signal seen in 2D multi-slice images due to different acquisition delay times [2]. Previously, it has also been shown in the context of projection angiography [3] and segmented acquisition FAIR and CASL approaches [4] that use of inversion pulses results in superior temporal stability of ΔM images by reducing the background signal. Other related works include 3D fMRI using single-shot spirals with FAIR [5] and 3D-GRASE with CASL [6] and with FAIR [7]. However, it is not clear whether the use of such inversion pulses will lead to quantifiable reduced temporal variation with single-shot 3D-TFEPI acquisition schemes. Our results indicate that the use of even a single non-selective inversion pulse (hyperbolic-secant pulse) leads to greatly improved background suppression and reduced temporal variability of ΔM images

Materials and Methods

The PULSAR sequence was modified as shown schematically in Figure 1. The two implementations were identical except that for IR-3D-PULSAR, following WET pre-saturation, “tagging” or “control” adiabatic inversion pulse(s) and post-saturation pulse, a non-selective inversion pulse was introduced. The TI time was determined by simulation so as to suppress CSF for the given TR. The modified sequence was implemented on a Philips 3T Achieva scanner (Release 1.5.4 software). Five healthy volunteers were scanned under an IRB approved protocol. IR-3D-PULSAR and 3D-PULSAR parameters were: TR/TD=2040/1500 ms; 60 pairs of control/label images; data acquisition: 3D-TFEPI with 24 slices, 4mm slice thick., 64x64 matrix, SENSE factor=2; DAC window≈450ms; scan time: 4 min 5 s. For IR-3D-PULSAR, the TI time was fixed at 720 ms prior to data acquisition. As shown in [4], introduction of N inversion pulses, results in $\Delta M^*(t) = (-1)^N \Delta M(t)$. Thus, $\Delta M^*(t)$ for the IR-3D-PULSAR acquisition was calculated using (Label – Control) instead of (Control – Label) images. The acquired $\Delta M(t)$ images were analyzed for temporal stability of the perfusion signal by calculating $\langle \sigma(\Delta M(t)) \rangle / \langle \Delta M(t) \rangle$ for ROIs in grey matter (GM), white matter (WM), CSF and for the whole brain (Glo). All ROIs and slices were matched for both sequences.

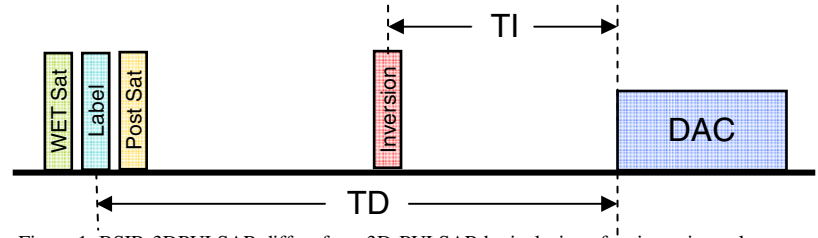


Figure 1: BSIR-3DPULSAR differs from 3D-PULSAR by inclusion of an inversion pulse.

Results

Figure 2 shows every fourth slice of the 24 slices acquired with IR-3D-PULSAR. Table 1 shows the values for $\langle \sigma(\Delta M(t)) \rangle / \langle \Delta M(t) \rangle$ averaged over all five volunteers. There was a considerable reduction in this measure for IR-3D-PULSAR as compared with 3D-PULSAR. Note that $\Delta M(t)$ values in WM and CSF were small, resulting in high ratios of $\langle \sigma(\Delta M(t)) \rangle / \langle \Delta M(t) \rangle$.

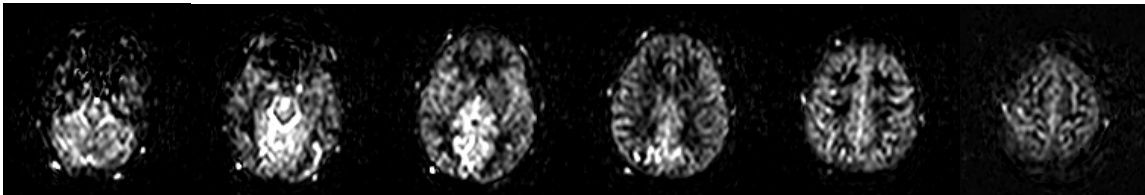


Figure 2: Every fourth slice of 24 slices acquired with IR-3D-PULSAR.

TABLE 1	$\langle \sigma(\Delta M_{GM}) \rangle / \langle \Delta M_{GM} \rangle$	$\langle \sigma(\Delta M_{WM}) \rangle / \langle \Delta M_{WM} \rangle$	$\langle \sigma(\Delta M_{CSF}) \rangle / \langle \Delta M_{CSF} \rangle$	$\langle \sigma(\Delta M_{Glo}) \rangle / \langle \Delta M_{Glo} \rangle$
3D-Pulsar	2.35±1.14	33.7±26.7	13.77±10.84	1.35±0.27
IR-3D-Pulsar	0.996±0.288	5.25±3.15	6.11±2.14	0.613±0.22

Conclusions

The inclusion of the inversion pulse in 3D-PULSAR results in higher temporal stability of ΔM images. The use of even a single inversion pulse between the tagging/control pulse(s) and data acquisition therefore proves greatly beneficial.

References

- [1] X. Golay et al. *MRM*, 53:15-21, 2005. [2] L. Talagala et al. *ISMRM*, 2006: 3422 [3] S. Mani et al. *MRM* 1997; 37:898-905. [4] F. Ye et al. *MRM*, 44 :92-100, 2000. [5] G. Duhamel et al., *ISMRM*, 2004: 518. [6] M. Fernandez-Seara et al. *MRM* 2005; 54: 1241-1247. [7] M. Günther et al. *MRM* 2005 ; 54 : 491-498.