

# Unified Mathematical Model of q-space and diffusion tensor imaging

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## Introduction:

Statistical imaging of random H<sub>2</sub>O motions using MRI has followed two mathematical paradigms: **diffusion-weighting** and **q-space** analyses. In diffusion-weighted analyses, the ensemble of molecules is assumed to evolve with a (not necessarily isotropic) Gaussian probability density/point spread function (PSF)—or a mixture of such densities—and the data analysis is oriented towards determining the parameters of the PSF (e.g., the apparent diffusion tensor). In q-space analyses, the transport is allowed to have a quite general PSF; as a result, much more data is required to reconstruct the PSF. The two analytical paradigms come from two different experimental communities with little overlap, since diffusion-weighted imaging is practicable in humans, whereas accurate q-space imaging is not. Our goal is to generalize the analysis of [1], which relates q-space and diffusion weighting.

## Analysis:

We denote by  $M(\mathbf{x}, t)$  the transverse magnetization and by  $\hat{M}(\mathbf{q}, t)$  its spatial Fourier transform. In the absence of magnetic field gradients, we model the transport of magnetization from its initial state  $M(\mathbf{x}, 0)$  to time  $t$  by convolution (\*) with an unknown time-dependent PSF  $P(\mathbf{x}, t)$ :

$$M(\mathbf{x}, 0) \xrightarrow{t} M(\mathbf{x}, 0) * P(\mathbf{x}, t) \Rightarrow \hat{M}(\mathbf{q}, 0) \xrightarrow{t} \hat{M}(\mathbf{q}, 0) \cdot \hat{P}(\mathbf{q}, t) \Rightarrow \frac{\partial \hat{M}(\mathbf{q}, t)}{\partial t} = \frac{\partial \hat{P}(\mathbf{q}, t)}{\partial t} \cdot \hat{M}(\mathbf{q}, t)$$

Define  $\hat{P}(\mathbf{q}, t) = e^{-u(\mathbf{q}, t)}$  (for diffusion,  $u(\mathbf{q}, t) = \mathbf{q} \cdot \mathbf{D} \cdot \mathbf{q} t$ , where  $\mathbf{D}$  is the diffusion tensor to be estimated), so that  $\hat{P}(\mathbf{q}, t)^{-1} \cdot \partial \hat{P}(\mathbf{q}, t) / \partial t = -\partial u(\mathbf{q}, t) / \partial t \equiv -u_t(\mathbf{q}, t)$ . With gradients,  $d\mathbf{q} / dt = \gamma \mathbf{G}(t)$ , and the magnetization transport model is:

$$\frac{\partial M(\mathbf{x}, t)}{\partial t} = -i \frac{d\mathbf{q}}{dt} \cdot \mathbf{x} M(\mathbf{x}, t) + \mathfrak{F}_{\mathbf{q} \leftrightarrow \mathbf{x}}^{-1} [-u_t(\mathbf{q}, t) \hat{M}(\mathbf{q}, t)] \Rightarrow \frac{\partial \hat{M}(\mathbf{q}, t)}{\partial t} - \frac{d\mathbf{q}}{dt} \cdot \nabla_{\mathbf{q}} \hat{M}(\mathbf{q}, t) = -u_t(\mathbf{q}, t) \hat{M}(\mathbf{q}, t)$$

The last equation is a first order PDE in  $(\mathbf{q}, t)$  space, which can be solved using the method of characteristics:

$\hat{M}(\mathbf{q}_0 - \mathbf{q}(t), t) = e^{-\int_0^t u_t(\mathbf{q}(\tau), \tau) d\tau} \hat{M}(\mathbf{q}_0, 0)$ , where  $\mathbf{q}_0$  is an arbitrary vector in q-space. For imaging purposes, the trajectory  $\mathbf{q}(t)$  is rewound to  $\mathbf{q} = \mathbf{0}$  at some time  $T$  before the  $k$ -space readout begins. Assuming that the  $k$ -space region covered is small enough not to induce significant diffusive effects itself, then we find that the attenuation of the image is given by

$E = e^{-\int_0^T u_t(\mathbf{q}(t), t) dt}$  or  $-\ln(E) = \int_0^T u_t(\mathbf{q}(t), t) dt = -\int_0^T [\hat{P}(\mathbf{q}(t), t)^{-1} \cdot \partial \hat{P}(\mathbf{q}(t), t) / \partial t] dt$ ; that is, a general trajectory through  $qt$ -space gives a tomographic result about the time evolution of the Fourier transform of the PSF for water transport.

## Discussion: qt-Space Tomography:

In the diffusion limit,  $\ln(E) = -\int_0^T \mathbf{q}(t) \cdot \mathbf{D} \cdot \mathbf{q}(t) dt$ , which is the basis for estimating the diffusion tensor  $\mathbf{D}$  by using different paths through  $qt$ -space. In the q-space PGSE experiment,  $T = \Delta$  and  $\mathbf{q}(t) = \text{const}$  (since the pulsed gradient duration  $\delta$  is assumed small), yielding  $E(\mathbf{q}) = e^{-\int_0^\Delta u_t(\mathbf{q}, t) dt} = e^{-u(\mathbf{q}, \Delta)} = \hat{P}(\mathbf{q}, \Delta)$ , the usual q-space imaging attenuation. If  $\delta$  is *not* small, then  $\mathbf{q}(t) \neq \text{const}$  and the relationship between  $E$  and  $\hat{P}(\mathbf{q}, t)$  is more complicated and involves all intermediate times  $0 \leq t \leq \Delta$ . If enough different trajectories through  $qt$ -space were traversed, *and* a parameterized mathematical model for  $\hat{P}(\mathbf{q}, t)$  adopted (cf. [2,3]), then the parameters of  $\hat{P}(\mathbf{q}, t)$  could be estimated from the  $-\ln(E)$  measurements. Such a technique may allow a systematic (if approximate) extension of q-space imaging to humans, where  $\delta$  cannot be small. Various extensions of this theory are possible, such as allowing for transport effects during excitation and for multiple coherent pathways through  $qt$ -space created by multiple RF pulses [4].

## References:

- [1] Basser PJ, *MRM* **47**: 392-397, 2002.
- [2] Özarslan E and Mareci TH, *MRM* **50**: 955-965, 2003.
- [3] Sato K-I, *Lévy Processes and Infinitely Divisible Distributions*, Cambridge, 1999.
- [4] Frank LR, Wong EC, Liu TT, and Buxton RB, *MRM* **49**: 1098-1105, 2003.

