Whole Blade Method for Robust PROPELLER DWI

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<u>INTRODUCTION</u>: Previous work for multicoil Diffusion Weighted PROPELLER FSE employs a "split blade" approach to compensate for the alternating motion related phase in even and odd spin echoes⁽¹⁾. This solution halves the effective blade widths, which make robust motion correction more difficult. Additionally, Figure 1 illustrates how a shift in k-space due to head rotation during DW gradient application may shift the k-space center near or beyond the edge of a narrow blade, resulting in image artifacts. The work proposed here is a new method for combining all echoes into one (wider) blade, which gives more robust signal, as illustrated in Fig. 1, as well as increasing the robustness of motion correction.



 $\begin{array}{l} \underline{\mathsf{DEFINITIONS:}} & \theta_m(\textbf{x}, \textbf{y}, \textbf{b}) = \text{phase from bulk motion during DW gradients; also varies for every blade b (e.g. every TR)} \\ & \theta_R(\textbf{x}, \textbf{y}, \textbf{c}) = \text{receiver phase; also varies for every coil c.} \\ & \theta_T(\textbf{x}, \textbf{y}) = \text{transmit phase for refocussing pulse (= initial signal phase right after 90° rf)} \\ & \theta_F(\textbf{x}, \textbf{y}, \textbf{k}) = \text{Fourier phase for encoding (also a function of k-space location k)} \end{array}$

<u>METHODS</u>: This method follows earlier work⁽²⁾ which alters even echoes by (1) reversing their applied phase encoding, (2) in recon flipping the data along k_x and then (3) conjugating the data, exploiting the relationship $f(x,y) = F(-k_x, -k_y)$. The odd echoes are used to fill the center of k-space (Fig. 1b), and the even echoes fill the outer edges. This results in

an image-space phase for collected <u>odd</u> echoes of θ_{ODD} an image-space phase for <u>collected even</u> echoes of an image-space phase for <u>conjugated even</u> echoes of $-\theta_{EVEN}$

$\theta_{ODD} = \theta_m(b,x,y) + \theta_T(x,y) - \theta_R(c,x,y) + \theta_F(x,y,k),$	[1]
$\theta_{\text{EVEN}} = -\theta_{\text{m}}(\mathbf{b}, \mathbf{x}, \mathbf{y}) + \theta_{\text{T}}(\mathbf{x}, \mathbf{y}) - \theta_{\text{R}}(\mathbf{c}, \mathbf{x}, \mathbf{y}) - \theta_{\text{F}}(\mathbf{x}, \mathbf{y}, \mathbf{k})$, and	d [2]
$\theta_{\text{EVEN}} = \theta_{\text{m}}(\mathbf{b}, \mathbf{x}, \mathbf{y}) - \theta_{\text{T}}(\mathbf{x}, \mathbf{y}) + \theta_{\text{R}}(\mathbf{c}, \mathbf{x}, \mathbf{y}) + \theta_{\text{F}}(\mathbf{x}, \mathbf{y}, \mathbf{k}).$	[3]

For each coil, the non-diffusion weighted (b=0) blades ($\theta_m = 0$) are averaged to estimate $\phi(\mathbf{c}, \mathbf{x}, \mathbf{y}) = \theta_T(\mathbf{x}, \mathbf{y}) - \theta_R(\mathbf{c}, \mathbf{x}, \mathbf{y})$. The two parts of each blade [center (odd echo) and edge (even echo)] are then transformed into image-space separately, and $\phi(\mathbf{c}, \mathbf{x}, \mathbf{y})$ is subtracted from the center data and added to the even data. The blade data are then added together, combined across coils, after which a standard method for estimating and removing $\theta_m(\mathbf{b}, \mathbf{x}, \mathbf{y})$ from each blade is employed, followed by conventional PROPELLER reconstruction.



REFERENCES: 1. ISMRM 2003, abstract #2126. 2. Mag Res Med 42: 963. ACKNOWLEDGMENTS: This work was funded in part by GE Healthcare.