

HOW LOW CAN WE GO? LIMITS OF DETECTION IN PASADENA ¹³C HYPERPOLARIZATION

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Objective: Fast ¹³C imaging at safe, physiological concentrations of water-soluble, non-toxic, hyperpolarized ¹³C contrast agents.

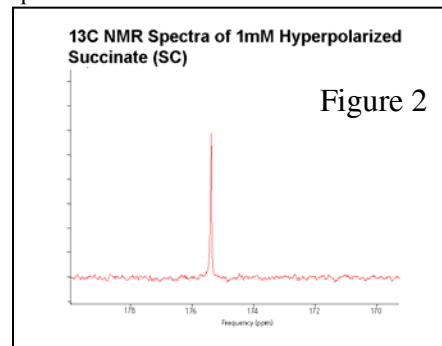
Background: *In vivo* ¹³C MRS of human brain defines concentrations of important fuels and neurotransmitters between 1-10 mM and reaction rates of 1-5 μmoles/min/gram. Two novel methods of hyperpolarization of ¹³C, dynamic nuclear polarization (DNP) and Parahydrogen and Synthesis Allow Dramatically Enhanced Nuclear Alignment (PASADENA); provide signal enhancement for ¹³C in excess of 10,000. Both techniques have shown utility in *in vivo* fast ¹³C imaging and spectroscopy and DNP is undergoing clinical trials. However, even after removal of toxic constituents and sterilization, the concentration of ¹³C pyruvate contrast agent employed (0.3M) will be 3000 times higher than physiological, presenting unacceptable biochemical and osmotic stress. Similarly, PASADENA (a.k.a. parahydrogen induced polarization: PHIP) ¹³C imaging, which was demonstrated initially with acetone-solutions, and later with aqueous solutions of a ¹³C reagent, employed a concentration (0.3M) 250 times higher than the known lethal dose (LD50 = 1.3mM). Last year, we demonstrate with PASADENA, that ¹³C imaging can be achieved as concentrations as low as 0.5 mM *in vitro* and 9 mM *in vivo*. This year, we have improved on the polarization of the molecules to go as low as 10μM *in vitro* and 100 μM (0.1 mM) *in vivo*. With the now achievable ¹³C signal enhancement of 100,000 fold, *in vivo* images of ¹³C metabolites comparable to those available from proton of water (80M) should permit contrast agent concentrations to be reduced to 1mM.

Materials and Methods: To facilitate routine PASADENA trials, GE Healthcare, Malmo has developed an automated polarizer for the initial steps of synthesis and polarization transfer, presently installed at the Huntington Medical Research Institutes, Pasadena. The polarizer was individually optimized for the production of two hyperpolarized water soluble molecules; a: 1- ¹³C hydroxyethylpropionate (HEP), b: 1- ¹³C sodium succinate (SC) was located at distinct positions to each MR instrument: (i) high resolution vertical bore Varian Mercury 7T NMR spectrometer, (ii) horizontal bore Bruker Avance 4.7T animal scanner, and (iii) 1.5T GE Signa clinical scanner, all equipped with ¹³C detection capability. Hyperpolarized ¹³C signal intensity was quantified with comparison to an internal ¹³C standard containing known concentration of 1- ¹³C sodium acetate.

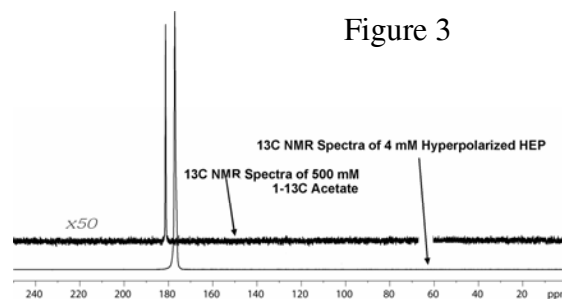
Results: Polarization of over 40% was obtained for HEP, while ~20% polarization was obtained for SC. Signal enhancement ranged between 18,000 and 100,000 (Table 1). Intensity of ¹³C images/spectra was linear and proportional to concentration. *In vitro* ¹³C spectra were readily produced at ¹³C concentrations as low as 10μM. Figure 1 shows an *in vivo* 3D FIESTA brain image of rat on injection of 25 mM solution of hyperpolarized ¹³C succinate (SC) via carotid artery. Figure 2 & 3 shows *in vitro* ¹³C NMR spectra of HEP and SC at millimolar concentrations.

| System | %STD | N | Signal Gain |
|--------------------|------|---|--------------|
| Bruker Avance 4.7T | 14% | 4 | 50,000 fold |
| GE Signa 1.5T | 9% | 2 | 101,000 fold |
| Varian Mercury 7T | 46% | 8 | 18,100 fold |

Table 1: Reproducibility of hyperpolarization with HEP



Discussion: PASADENA lends itself to rapid generation of hyperpolarized ¹³C reagents for studies necessary to establish dose-response curves *in vitro* and *in vivo*. As was theoretically anticipated, the signal enhancement achieved by routine hyperpolarization was sufficient to permit detection hyperpolarized ¹³C reagents for studies necessary to establish dose-response curves *in vitro* and *in vivo*. The signal enhancement achieved by routine hyperpolarization was sufficient to permit detection of ¹³C concentrations as low as 0.01 mM. Somewhat higher ¹³C concentration, 0.1 mM, necessary for *in vivo* imaging are in part a function of the additional time taken for injection. Allowing a dilution factor of 4 – 12 fold when contrast agent is mixed with circulating blood, results *in vivo* and *in vitro* were comparable. Our previous estimate of the limit of detection (9mM) was far above the relevant physiological concentration of most biological compounds. We can now estimate the “limit” to be an order of magnitude lower and within the physiological concentrations of most biochemical processes.



Conclusion: *In vivo* PASADENA ¹³C imaging with hyperpolarized contrast agents can be achieved using near/under physiological concentrations of naturally occurring metabolites and relevant unsaturated bio-molecules.

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References: a) P. Bhattacharya, K. Harris, A.P. Lin, M. Mansson, V.A. Norton, W.H. Perman, D.P. Weitekamp, and B.D. Ross, *MAGMA* 18 (2005) 245-256. b) Bhattacharya, P. K.; Chekmenev, E. Y.; Harris, K.; Weitekamp, D. P.; Tan, C. T.; Ross, B. D. *JMR* (2006) submitted.