

## Temporal variability of $R_2^*$ estimates in single-shot methods

H. Deshpande<sup>1</sup>, D. B. Twieg<sup>1</sup>

<sup>1</sup>Biomedical Engineering / Center for Development of Functional Imaging, University of Alabama at Birmingham, Birmingham, Alabama, United States

### Introduction

In functional MRI (fMRI), typically a series of images are acquired in rapid succession during a cycle of control and stimulation to detect activity changes in regions of the brain. These activity changes are signified by changes in tissue  $R_2^*$ , caused by the Blood Oxygenation Level Dependent (BOLD) mechanism. In most fMRI experiments,  $\Delta R_2^*$  is not measured directly, but is inferred from signal changes in serial  $T_2^*$ -weighted EPI images. A potentially more accurate method of measuring changes in  $R_2^*$  is the multiple-gradient echo EPI method (MEPI), which acquires separate EPI images at several echo times following a single excitation, allowing an exponential fit to be made to compute  $R_2^*$ . A recently introduced technique for  $R_2^*$  measurement, single-shot parameter assessment from signal encoding (SS-PARSE) maps  $R_2^*$ , frequency ( $\omega$ ) and local magnetization  $M_0$  by modeling the local signal and solving an inverse problem [1]. Because it explicitly models local phase evolution during the signal, it is inherently free of off-resonance geometric distortion. The sensitivity and accuracy of fMRI depend critically on the ability to measure small changes in  $R_2^*$ . To compare the temporal variability of  $R_2^*$  estimates using MEPI and SS-PARSE, repeatability studies were performed using phantoms with a range of  $R_2^*$  values.

### Method

The SS-PARSE method uses a model which is based on the local signal from each pixel,

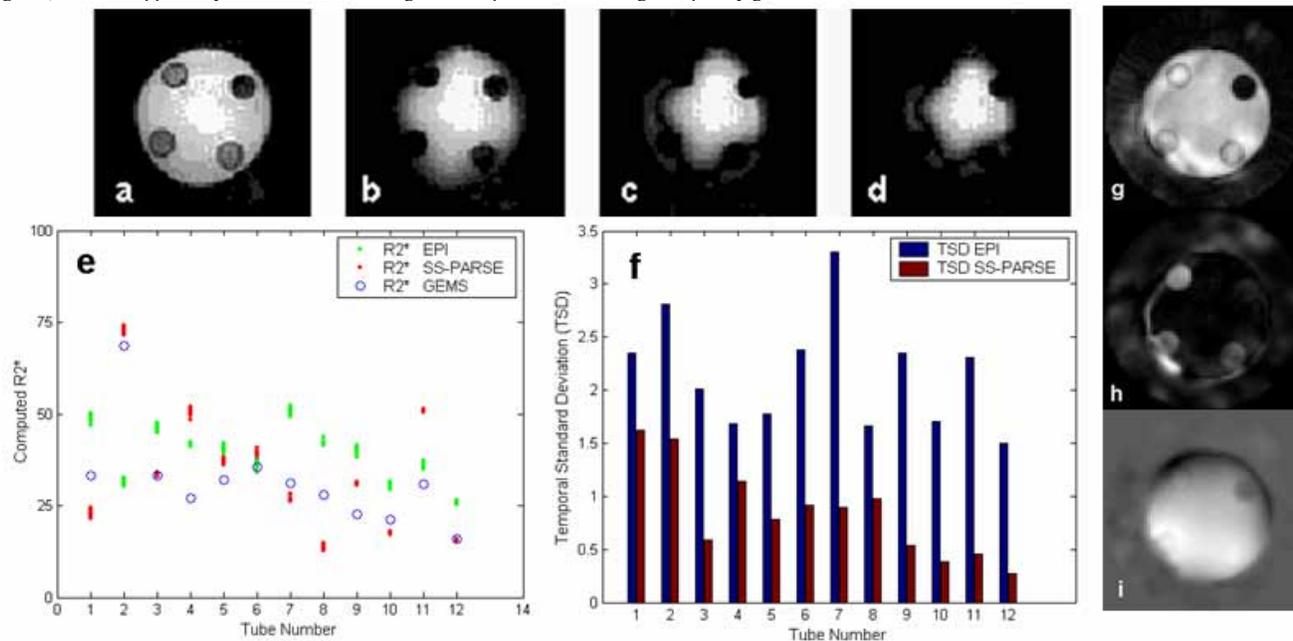
$$S_{n_j} = M_0 e^{-2\pi(k_{xn}x_j + k_{yn}y_j)} e^{-(R_2^* + i\omega)n\Delta t}$$

and determines by conjugate gradient search the set of pixel parameters  $M_0$ ,  $R_2^*$ , and  $\omega$  ( $j=1, \dots, J$ ) best matching the total signal observed to the sum of the local signals,  $s_n = \sum_j s_{n_j}$ . Here the  $j^{\text{th}}$  pixel is at  $(x_j, y_j)$  and  $k_{xn}, k_{yn}$  represent the  $k$ -trajectory at time  $n\Delta t$ .

Phantom studies for  $R_2^*$  estimation were performed on a Varian 4.7-T vertical 60-cm-bore scanner. Each study consisted of 4 tubes containing an aqueous solution of agar and different concentrations of sephadex and copper sulphate which gave varying values of  $R_2^*$ . Initially a series of gradient echo (GEMS) images,  $128 \times 128$  image resolution, slice thickness = 3mm, TR = 90 ms, and 13 values of TE = 5, 10, 15, 20, 25, 30, 35, 40, 45, 50, 60, 70, 80 ms, were acquired. The  $R_2^*$  values obtained through this series were used as standard for comparison. A series of MEPI images,  $64 \times 64$  image resolution, slice thickness = 3mm, TR/TE = 3000/22.8 ms, each with 4 echoes was repeated 32 times. Next, a SS-PARSE acquisition, thickness = 3mm, TR = 3000 ms, was repeated 32 times. The MEPI and SS-PARSE data sets with 32 repetitions each, were used for the task of evaluating the temporal standard deviation (TSD). All regions of interest selected were  $4 \times 4$  pixels and were entirely within the tubes.

### Results

For pixels within the selected regions of interest, TSD for SSPARSE estimates were significantly lower than TSD for the MEPI method (fig. 1.f).  $R_2^*$  estimates by both MEPI and SSPARSE occasionally deviated significantly from the actual values, but there was no systematic bias which would affect the TSD values. Note in the  $R_2^*$  map (fig. 1.h) a rim of apparently elevated  $R_2^*$  near edges of the phantom with large frequency gradients.



**Fig. 1.** a-d: EPI intensity images spaced by 22.8 ms echoes; e: Computed  $R_2^*$  values for gradient echo, SS-PARSE (20 frames), and MEPI(20 frames) in each of the 4 tubes from 3 experiments; f: Comparison between SS-PARSE and MEPI in terms of their TSD values in 4 tubes from 3 experiments over 20 frames; g: Intensity image ( $M_0$  map), h:  $R_2^*$  map, and i: Frequency map computed using SS-PARSE technique from a single shot

### Discussion

A single-shot method for estimation of  $R_2^*$  without off-resonance distortion was created and validated with phantom studies. SS-PARSE  $R_2^*$  estimates matched more closely than MEPI estimates from gradient echo studies. Additional advantages of this method come in the form of magnitude, and frequency information, both of which are obtained using a single-shot. Since the  $R_2^*$  values obtained using SS-PARSE show lower variability over time, it appears suitable for fMRI studies which rely on the repeatability of the results within the duration of the designed experiment.

### Acknowledgements

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### References

1. Twieg DB. Magn Reson Med 2003;50:1043-105