

A Double-Resonant $^{19}\text{F}/^1\text{H}$ Transmit/Receive Solenoid Coil for MRI

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Introduction

^{19}F MR imaging has a high potential for the detection and direct quantification of fluorine-labeled tracers and drugs in the field of molecular imaging [1]. The combination with ^1H imaging provides associated anatomical information. So far, this application has been typically supported by separate ^{19}F and ^1H RF-coils [2,3]. The sensitivity profiles of the coils differ at these two frequencies, so that the measured ^{19}F data cannot be corrected using the obtained ^1H data. We demonstrate a new $^{19}\text{F}/^1\text{H}$ double resonant solenoid transmit/receive coil for 3T, which exhibits practically the same sensitivity profile for both frequencies. This allows the correction of B_1 inhomogeneities in the ^{19}F image via the ^1H sensitivity profile.

Materials and Methods

We based our design on a solenoid with an inner diameter of 70 mm. The coil is built from strip conductors wound around a fiberglass cylinder. The gap between the individual strip conductors is 8 mm (Fig. 1). The overall inductance of the solenoid is $L_s=1024\ \mu\text{H}$ at 124 MHz. For further calculations, this value is assumed to be constant over a bandwidth of 20 MHz.



Fig. 1: Solenoid RF-coil using strip conductors fixed on a fiberglass cylinder.

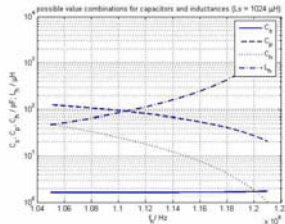


Fig. 2: Possible values for the double resonant coil (120.23 MHz, 127.73 MHz). Each value stack of a column gives a correct configuration.

Equidistant splits with 15 capacitors ($15 \cdot C_s$) were introduced along the conductor to avoid current inhomogeneities by propagation effects. An additional split is used to include one parallel LC-circuit (C_p , C_h , L_h) in series with the coil conductor. The current of this parallel circuit does not influence the B_1 -field profile of the solenoid. While the series circuit of L_s and C_s behaves like a capacitor ($\text{imag}\{Z\} < 0$) for frequencies below the resonance frequency and like an inductance ($\text{imag}\{Z\} > 0$) for higher frequencies, the parallel circuit behaves the opposite way. The solenoid can be tuned to resonate at the 3T Larmor-frequencies of ^{19}F (120.23 MHz) and ^1H (127.73 MHz) via selection of the circuit components.

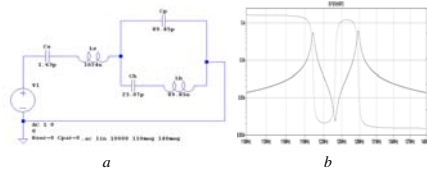


Fig. 3: Circuit diagram of the solenoid (L_s , C_s) and the implemented parallel circuit (C_p , C_h , L_h) (left). Simulated input impedance as function of frequency for a lumped element model (right).

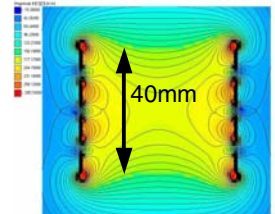


Fig. 4: Cross-section of the B_1 -profile (^1H , ^{19}F) simulated with an EM-full-wave tool (FEKO).

double resonance for $^1\text{H}/^{19}\text{F}$. The values for the capacitors and inductances were selected according to the simulation results (Fig. 3). Scans to verify the matching of the B_1 profile were performed on a 3T whole-body MR scanner (Achieva, Philips Medical Systems: FOV 70 mm, 128x128 matrix (0.54 mm pix), TR/TE = 17.4 ms/8.7 ms, 19 coronal slices à 2 mm, readout R/L, pixel BW 98.6 Hz).

Results and Discussion

The unloaded quality factor of the double tuned RF-coil was measured to be approximately $Q=400$ (Fig. 5b). Input impedance and transmission behavior was measured to be in good agreement with simulation (cf. Fig. 3b vs. Fig. 5c). Variable capacitors were used for fine-tuning. The measured input impedance after fine-tuning is shown in Fig. 5a. A good $50\ \Omega$ matching could be achieved for both frequencies 120.23 MHz and 127.73 MHz.

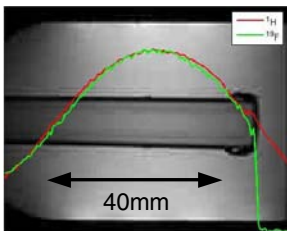


Fig. 6: Reconstructed $^{19}\text{F}/^1\text{H}$ -image acquired with double resonant coil. No influence of parallel circuit can be seen

^{19}F and ^1H images from a phantom are shown in Fig. 6. The inner cylinder contains ^{19}F in Perfluoro-Crown-Ether and is surrounded by water. Signal intensity profiles through the ^{19}F -fluid (green) and through water (red), normalized on the maximum, demonstrate the predicted agreement of both sensitivity profiles.

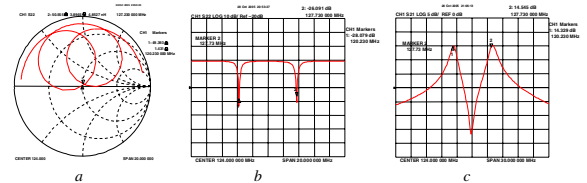


Fig. 5: Input impedance of the double resonant solenoid (left, mid) measured on a network analyzer. Transmission behavior (S_{21}) displayed in a logarithmic scale (right). Matching to $50\ \Omega$ is achieved for both frequencies, i.e. 120.23 MHz and 127.73MHz.

Conclusion

A new $^{19}\text{F}/^1\text{H}$ double resonant transmit/receive solenoid coil for MRI imaging was designed. The sensitivity profile for ^{19}F and ^1H is practically identical. The double-resonant coil allows small animal studies in contrast agent and drug research.

References

- [1] Morawski A et al., MRM 52:1255 (2004)
- [2] Gonen O et al., MRM 37:164 (1997)
- [3] Krems B et al., Magn Reson B 108:155 (1995)