

# Restoration of EPI Susceptibility Distortion at 3T: Comparison of Fluid-Dynamic Image Registration with Phase-Encoding Gradient Reversion

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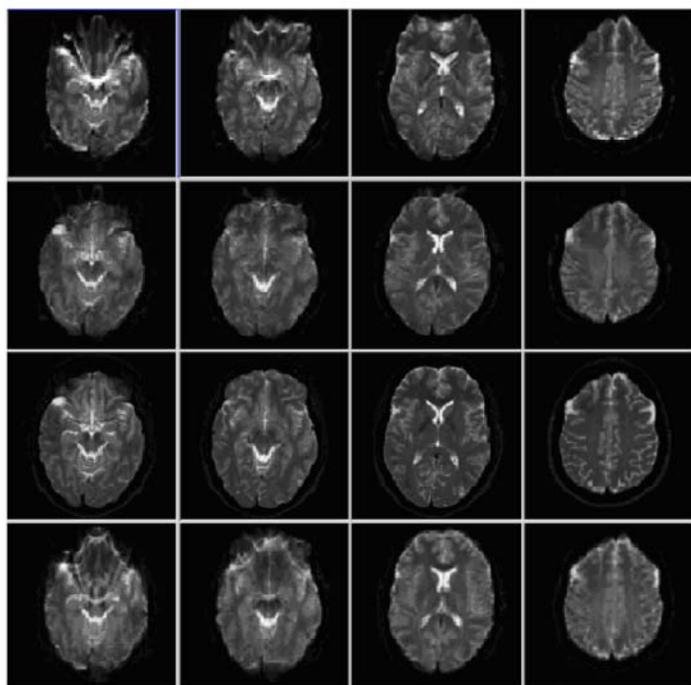
**Introduction.** We propose a cross evaluation of restoration methods for echo planar images acquired at 3 T, where the effect of susceptibility distortions is rather conspicuous. Two methodological strategies were tested to un-distort the images: (i) image registration of the distorted image with an undistorted (reference) image that has a similar contrast [1, 2], and (ii) co-registration of two distorted images – acquired with phase-encoding gradients of opposite sign [3, 4, 5]. To assess the restoration success, tests included phantom experiments as well as *in vivo* imaging of the normal human brain. Results of the methods are compared using undistorted reference images, or, in case of the phantom, compared with the known structure.

**Methods.** All experiments were performed at 3T (MAGNETOM Trio, Siemens, Erlangen, Germany) using a standard birdcage headcoil. The amount of distortions was investigated with a blipped spin-echo EPI sequence ( $TR$  4 s,  $TE$  86.2 ms, bandwidth 1000 Hz/pixel,  $128 \times 128$  or  $64 \times 64$  acquisition matrix, half-Fourier reconstruction, 10 averages) with frequency-selective fat saturation. Two series of images were recorded with reversed phase-encoding directions (right to left and left to right or anterior to posterior and posterior to anterior in the phantom and *in vivo* experiments, respectively). A typical level of Nyquist ghosts was 1.6% of the object's image intensity.

A structured water phantom consisting of a cylindrical 1-L borosilicate glass beaker (DURAN, Schott, Mainz, Germany) with additional vertically oriented polyethylene tubes (1.2-mm wall thickness, 15-mm external diameter) of similar length as the beaker was used for the *in vitro* studies. The phantom was filled with aqueous NaCl solution (1.712 mol/L) and centered in the imaging coil in an upright position. The 2D images were oriented perpendicularly to the beaker's long axis in the phantom study (i.e., along the  $y$ -direction) with a field of view (FOV) of 128 mm. With this orientation, potential distortions along the slice-selection direction had no visible effect on the images due to the symmetry of the phantom.

*In vivo* brain images were recorded in healthy young human volunteers after informed written consent had been obtained. The 2D images were oriented along the bicommissural plane (AC-PC), and the FOV was 192 mm (slice thickness 4 mm, gap 1 mm). In all experiments, automated shimming was performed to minimize large-scale magnetic field inhomogeneities. Subsequently, spin-warp reference images were recorded with phase-encoding from right to left using proton-density and T2-weighted RARE sequences ( $TR$  4 s,  $TE$  12 or 103 ms, refocusing pulses  $150^\circ$ , RARE factors of 7 or 9, bandwidth 100 Hz/pixel, matrix  $256 \times 256$ , 2 averages).

**Results & Discussion.** From mere visual inspection (Fig. 1) results obtained by fluid-dynamic image registration schemes appear to be better than those obtained using reversed-gradient methods, because they account for large displacements and are able to correct for distortions in slice select gradient direction, too. A closer inspection of the (computed) distortion field revealed implausible reconstruction, primarily in read-out direction. This effect is not in accordance with susceptibility distortion on SE-EPI images, and requires to be taken under control. Since susceptibility distortions increase with field strength, we suppose that fluid-dynamic registration may be the better solution to estimate the distortion field at 3 T or above, especially for high-resolution imaging.



It may be interesting to modify fluid-dynamic image registration to implement a fluid-dynamic regularization for reversed-gradient methods to unify the advantages of a reconstruction based on the information from both images and the feature of the fluid registration to account for large displacements.

## References

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**Figure 1.** Comparison of distorted EPI images (top row) with results after fluid-dynamic registration (2<sup>nd</sup> row), undistorted RARE images (3<sup>rd</sup> row), and results from reversed-gradient correction (bottom row).