

Long-T₂ Imaging: Evidence of a New Water Reservoir in Multiple Sclerosis

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Introduction

In normal human white matter, water protons can be separated into three pools based on their T₂ relaxation times [1,2]. The longest T₂ component (2s) is due to cerebrospinal fluid, an intermediate component (80-100ms) arises from intra/extracellular (IE) water and the shortest T₂ component (20ms) is due to water trapped between the myelin bilayer (myelin water). Previous T₂ relaxation work in multiple sclerosis has shown abnormalities in the T₂ distribution in terms of total water content and myelin water fraction (MWF) for both normal appearing white matter (NAWM) and lesions [3]. Two previous studies using spectroscopy [4] and multi-echo T₂ relaxation (TE=30ms) [5] reported the presence of an additional longer T₂ component in MS lesions. The purpose of this study was to better define the T₂ distribution in MS lesions and NAWM with particular emphasis on identifying potential long T₂ components, by lengthening the total acquisition time of the multi-echo T₂ relaxation sequence from 320ms to 1.120s, with the ultimate aim being to better characterize lesions on the basis of their pathology.

Methods

Subject Information: Twenty subjects with clinically definite MS underwent MR examinations (14 relapsing-remitting, 3 secondary-progressive, 2 relapsing-progressive, 1 benign; 15 female, 5 male; median EDSS = 2.5 (range 1.0-8.0); mean age = 38yrs (range 23-54yrs); mean disease duration = 10.5yrs (range 1-35yrs)).
MR Experiments: MR experiments were conducted on a 1.5T GE Echo Speed scanner operating at the 5.7 software level. Localizers, proton density and T₂ images (TR 2500 ms, TE 30/80 ms) were followed by a 48 echo modified Carr-Purcell-Meiboom-Gill (CPMG) sequence with variable TR, consisting of a 90° slice selective pulse followed by 48 rectangular composite 180° pulses flanked by slice-selective crusher gradient pulses for elimination of stimulated echoes [6]. For the CPMG T₂ relaxation measurement, a single transverse slice was acquired (TR = 2120-3800ms, TE = first 32 echoes @ 10ms, last 16 echoes @ 50ms, 5 mm thick, 256x128, 4 averages). A post Gd-DTPA T₁-weighted spin echo series (TR 550ms, TE 8ms, 22 slices, matrix 256x192) was also collected.
Data Analysis: Regions of interest (ROIs) were outlined around lesions and contralateral NAWM. T₂ relaxation decay curves were decomposed into an unspecified number of exponentials using a regularized non-negative least squares algorithm using 120 input relaxation times spaced logarithmically from 15ms to 2s [7]. Both χ^2 and solution roughness were minimized such that χ^2 fell between 1.02 and 1.025 times the minimum χ^2 from the non-regularized least-squares solution. Results were displayed as a T₂ distribution plot of component amplitude as a function of T₂. Geometric mean T₂ (GMT₂) and peak width (analogous to the variance on a logarithmic scale) of the IE component from 50ms to 200ms and the potential Long-T₂ component from 200ms-800ms were calculated. The MWF was defined as the fraction of the T₂ signal below 50ms relative to the total signal in the T₂ distribution. Similar to the MWF, a "Long-T₂" component fraction was calculated by dividing the T₂ signal between 200 and 800 ms by the total signal in the T₂ distribution. MWF and Long-T₂ maps were created for each subject by calculating the fraction of each component for every pixel in the image. Statistical analysis was carried out using a two-tailed Student's t test with a p value of <0.05 considered significant. All errors are expressed as standard errors.

Results

A total of 92 lesions and 92 contralateral NAWM areas were examined in the 20 subjects with MS. On average, MWF for all lesions was 0.046 (0.004), 39.2% less (p<0.0001) than average NAWM MWF, 0.076 (0.006). IE GMT₂ for all lesions was on average 119ms (3ms), 38.5% longer (p<0.0001) than average NAWM GMT₂, 86ms (1ms). The average width of the IE peak for lesions was 0.17 (0.04), 40% wider (not significant, p=0.16) than average NAWM peak width of 0.12 (0.02). Signal from a Long-T₂ peak between 200ms and 800ms was identifiable in 28 lesions from 11 subjects. The average MWF of those Long-T₂ lesions was 0.039 (0.007), less, although not significantly different (p=0.14) from, the average MWF of those 64 lesions which had no Long-T₂ component 0.049 (0.004). The average IE GMT₂ for Long-T₂ lesions was 132ms (6ms), longer (p=0.0009) than the average IE GMT₂ of the lesions with no Long-T₂ signal, 113ms (2ms). The average GMT₂ of the Long-T₂ peak itself was 280ms (23ms). A wide heterogeneity was observed in Long-T₂ peak fraction for each lesion, with a median value of 0.076 (0.058). A Long-T₂ peak (average fraction 0.029 (0.011)) was also observed in 3 NAWM areas in 2 different subjects. Of the 92 lesions, 5 were gadolinium enhancing. 2 of the 5 enhancing lesions showed a Long-T₂ peak and average values for MWF, IE GMT₂ and peak width were not different from non-enhancing lesions. Figure 1 shows a PD, Gad-T₁, myelin map and Long-T₂ map for an MS patient with an enhancing lesion. Three ROIs with corresponding T₂ distributions are shown for the enhancing core of the lesion, non-enhancing periphery and NAWM. Figure 2 shows images from 2 other subjects demonstrating the Long-T₂ component.

Conclusions

Our goal was to better characterize the T₂ distribution in MS white matter. As expected, decreased myelin water, increased GMT₂ and increased peak width of the intra/extracellular (IE) peak were observed in MS lesions. Of particular interest, a new water reservoir with a markedly prolonged T₂ peak (200-800ms) was also identified in 30% of lesions and several NAWM regions. This peak is possibly due to increased extracellular water and has also been identified in PKU [8]. Those lesions with a Long-T₂ peak also exhibited longer IE GMT₂ than those lesions without a Long-T₂ signal.

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References

1. MacKay, AL, Whittall, KP, Adler, J et al. MRM, 31 673-7, 1994.
2. Whittall, KP, MacKay, AL, Graeb, DA et al. MRM, 37,34-43, 1997.
3. Laule C, Vavasour IM, Moore GRW et al. J Neurol. 2004;251:284-293.
4. Helms G. MRM 2001; 46:256-263
5. Larsson HBW et al. MRM 1988;7:43-55
6. Laule C, Whittall KP, and MacKay AL. ISMRM, Glasgow, 2001, p 896.
7. Whittall KP, MacKay AL. J Magn Reson 1989;84:134-152
8. Laule C, Tahir SA, Brief EE et al. Submitted Abstract to ISMRM 2006

