

# Accurate, $B_1$ -Insensitive Fast $T_1$ -Measurements at 3T

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## Introduction

Fast  $T_1$ -measurements can be acquired in a few seconds using the Look-Locker principle in conjunction with echo-planar imaging. [1,2] Accurate calculation of  $T_1$ , however, requires knowledge of the true mean flip angle through a slice [3], which varies throughout the imaged volume due to  $B_1$ -inhomogeneities. The flip angle cannot be estimated by fitting the signal model to measured data since it is strongly correlated to other parameters in the model. However, by repeating the  $T_1$ -measurement with multiple flip angles, it is possible to estimate the flip angle along with  $T_1$ ,  $M_0$  and the degree of inversion,  $\beta$ . This allows accurate and fast measurement of  $T_1$  in the presence of  $B_1$ -inhomogeneities.

## Methods

Look-Locker  $T_1$ -measurements were acquired in a single slice in both a homogenous gel phantom and a human subject. All measurements were done on a Siemens Magnetom Trio 3T-scanner. GE-EPI was used for imaging and a non-selective hyperbolic secant adiabatic inversion pulse was used for inversion with  $TI=50$ ms. The measurements were repeated with two flip angles. For the phantom measurements, flip angles,  $\alpha$  of  $10^\circ$  and  $15^\circ$  were used and the time between slices,  $\delta TI$ , was 75ms. For the in-vivo measurements  $\alpha$  was  $15^\circ$  and  $25^\circ$  and  $\delta TI$  was 200ms.

A four-parameter model with the unknowns  $T_1$ ,  $M_0$ ,  $\alpha$  and  $\beta$  was fit to the data acquired with both flip angles. It was assumed that the ratio between the actual flip angles in the two measurements was constant regardless of the  $B_1$ -inhomogeneities.

## Results

Figure 1 shows the fitted ratio between the actual and nominal flip angles in both the phantom and in-vivo measurements. The ratio shows good agreement with a typical  $B_1$ -map. Figure 2 shows histograms of the fitted  $T_1$  values in the homogenous phantom with the normal single-flip-angle Look-Locker method (for  $\alpha=10^\circ$  and  $15^\circ$ ) as well as with the proposed 2-flip-angle method. The proposed method clearly has a narrower histogram indicating more robust  $T_1$  estimation. Figures 3&4 show the corresponding  $T_1$ -maps and histograms for the in-vivo measurements where it can be seen that the histogram with the 2-flip-angle method is narrower than with the single-flip-angle method. The accuracy of the fitted  $T_1$ -maps could potentially be further improved by constraining the  $B_1$ -maps to be smooth, e.g. by using a masked polynomial fit to smooth the fitted flip-angles.

## Conclusions

It was shown that  $B_1$ -insensitive fast  $T_1$ -measurements can be acquired using the Look-Locker method by using two flip angles and fitting an appropriate model to the measured data. This improves the accuracy of  $T_1$ -measurements at especially high field where  $B_1$ -inhomogeneities are pronounced.

## References

- [1] Look,DC and Locker,DR. Rev Sci Instrum 1970;41:250-1.
- [2] Gowland,P and Mansfield,P. Magn Reson Med 1993;30:351-354.
- [3] Sidaros,K et al. Proc. 8<sup>th</sup> ISMRM 2000;p.429

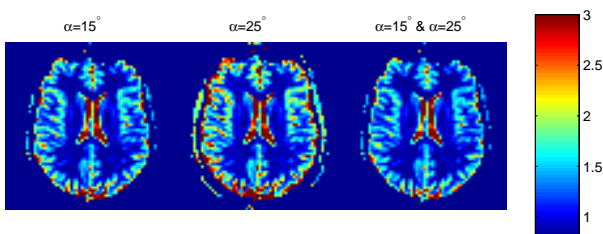


Figure 3:  $T_1$ -maps [s] obtained with the single-flip-angle LL method (left and middle) and with the proposed 2-flip-angle method (right).

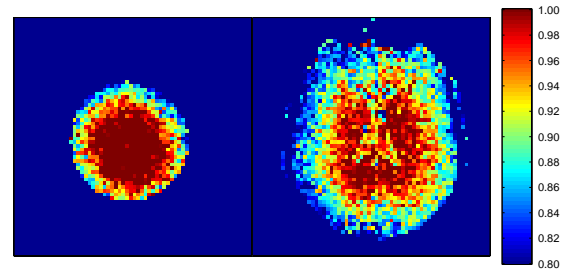


Figure 1: The ratio between the actual and the nominal flip angles in a phantom (left) and in-vivo (right).

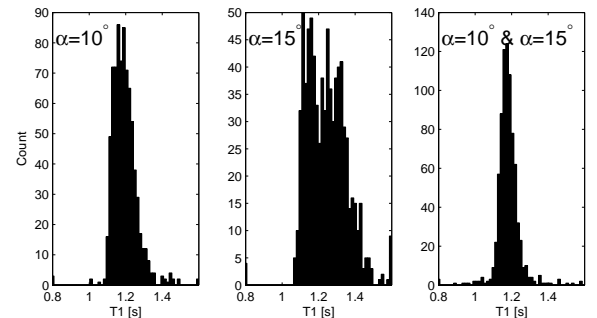


Figure 2: Histograms of the fitted  $T_1$  values in a phantom with the single-flip-angle LL method (left and middle) and with the proposed 2-flip-angle method (right).

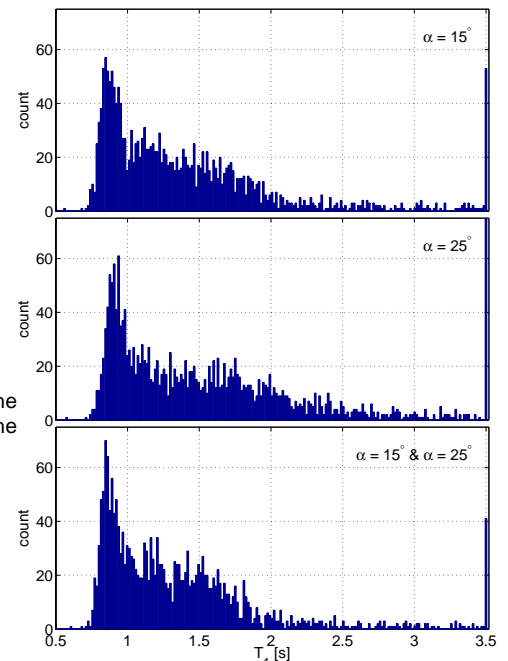


Figure 4: Histograms of the fitted  $T_1$  values shown in the maps in figure 3.