

# Effects of magnetic circuits on magnetic field gradients produced by planar gradient coils

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## Abstract

Effects of magnetic circuits on magnetic field gradients produced by planar gradient coils were measured for two MRI permanent magnets. As a result, it was found that the enhancement rates of the magnetic field gradients were different among x, y, and z directions. The difference gave us useful information on the mechanism of the gradient field enhancement phenomena.

## Introduction

Magnetic field gradients produced by gradient coils in MRI permanent magnets are enhanced due to the presence of magnetic materials. The enhancement mechanism has been theoretically analyzed using a mirror-current approach and the finite element method [1]. However, as far as we know, there is no experimental report on this subject. In the present study, we measured magnetic field gradients produced by a planar gradient coil set in a free space and in gap spaces of two MRI permanent magnets and found that the yoke must be considered to calculate the enhancement rate.

## Materials and methods

A planar gradient coil set was designed according to the target field method [2, 3]. The design parameters were as follows: magnet gap: 16 cm, target region: 12 cm dsv, diameter of the current flowing region: 34 cm, number of turns of wires: 25 for G<sub>x</sub> and G<sub>y</sub>, 28 for G<sub>z</sub>. Each gradient coil element was wound on a 0.5 mm thick FRP plate using a 1.0 mm diameter polyethylene coated Cu wire. The 3-axis gradient coil assembly was made by piling up the G<sub>y</sub> and G<sub>z</sub> coils on the G<sub>x</sub> coils (Fig.1). Two permanent magnets were used for the measurements: a C shaped magnetic circuit (Fig.2), field strength; 0.21 T, gap; 25 cm, pole-piece diameter; 52cm, and a magnetic circuit with two columns (Fig.3), field strength; 0.21 T, gap; 16 cm, pole-piece diameter; 40cm. The gradient coil set was placed in a free space and the magnetic field distribution was measured using a Hall magnetometer. The gradient coil set was then fixed in the magnet gap spaces and the gradient fields were measured using water phantoms and 3D imaging sequences.

## Results and discussion

Table 1 shows the efficiency of the gradient coils obtained from a numerical calculation and the measurements. Agreement between the calculation and the measurement in a free space is good. The enhancement rates can be roughly explained by the mirror-current theory for the pole-pieces [1]. However, those of the G<sub>z</sub> coil are definitely smaller than those of the G<sub>x</sub> and G<sub>y</sub> coils. This result suggests that the effect of the yoke must be considered for the enhancement-rate calculation for the G<sub>z</sub> coil, because the magnetic flux generated by one piece of the G<sub>z</sub> coil set tries to decrease the magnetic flux generated by the other piece of the G<sub>z</sub> coil set through the yoke. For G<sub>x</sub> and G<sub>y</sub> coils, however, there is no such interaction. Figure 4 shows images of a phantom acquired in the xz plane in the two magnets. Because the image distortion observed for the 16cm-gap magnet is slightly larger than that for the 25cm-gap magnet, the pole-piece degrades the homogeneity of the gradient fields. In conclusion, for the enhancement-rate calculation of planar gradient coils for permanent magnets, the presence of yoke must be considered for G<sub>z</sub> coils.

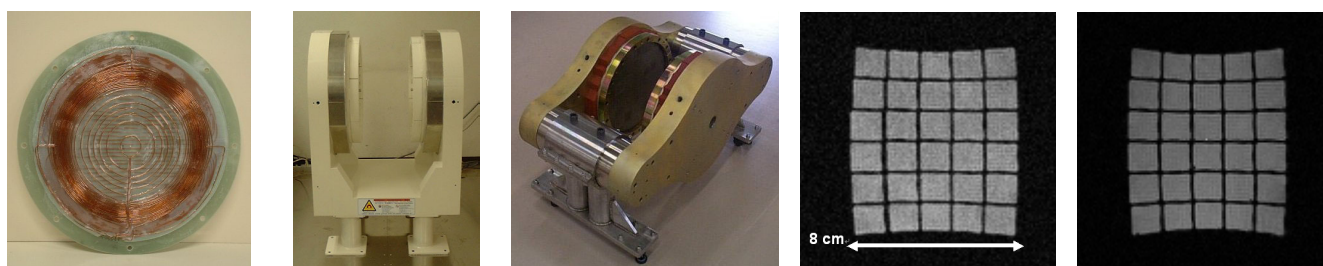


Fig.1 Planar gradient coil set Fig.2 C shaped magnet Fig.3 Two column magnet Fig.4 Phantom images (L: with C shaped, R: with two column)

	Calculation	Free space	C shaped magnet	Two column magnet
G <sub>x</sub>	0.0963 (1.01)	0.095	0.110 (1.16)	0.168 (1.77)
G <sub>y</sub>	0.0931 (1.02)	0.091	0.107 (1.18)	0.168 (1.85)
G <sub>z</sub>	0.191 (0.97)	0.196	0.216 (1.10)	0.319 (1.63)

Table 1. Efficiency of the gradient coils ( $G \text{ cm}^{-1} \text{ A}^{-1}$ ). Numbers in the parentheses are values normalized by those measured in a free space.

## References

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