

# Imaging the evolution of 3-D myocardial strains using a combined HARP-SENC MRI pulse sequence

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## Introduction

The development of a rapid 3-D strain imaging and post-processing system with high temporal resolutions still remains a challenge. We present a pulse sequence that combines two tag based magnetic resonance imaging methodologies — harmonic phase (HARP) [1] and strain encoded (SENC) [2] — to provide rapid dense 3-D strain imaging for a stack of short-axis slices in one-two short breath-holds. Using the pulse sequence, evolutions of 2-D in-plane normal strains (circumferential and radial) and 1-D out-of-plane normal strains (longitudinal) can be computed for a stack of  $n$  contiguous short-axis slices prescribed in the left ventricle from data acquired in a single breath-hold lasting  $6n$  heartbeats.

## The Imaging Technique

This new pulse sequence, called HARP-SENC MRI [3], was designed and tested on a 1.5T Signa CV/i whole body MR system (GE Medical Systems, Waukesha, WI). A typical HARP-SENC MRI scan requires a six-heartbeat acquisition for each slice (See Fig. 1). Multiple slices are acquired in a sequential fashion. At the beginning of each heartbeat, specialized 1-1 SPAMM tags are applied at end-diastole. During the first and second heartbeat, reference datasets are acquired for phase-sensitive reconstruction of the four-channel receiver coil data [8]. The third and fourth heartbeats are then used to acquire the harmonic images and during the fifth and sixth heartbeats, the SENC images are acquired at tuning frequencies  $s1$  and  $s2$  respectively. During each heartbeat, a four-shot interleaved gradient-echo based echo planar imaging scheme is employed to acquire small regions of interest of size  $32 \times 32$  around the spectral peak of interest. An incrementing train of imaging flip angles is also employed to prevent the characteristic tag decay due to the imaging pulses. Typically, a CINE sequence of around 10-15 images are acquired every heartbeat, each with a temporal resolution of 38.8ms. Data presented in this abstract is from a normal volunteer. Five SA axis slices were prescribed with a field-of-view of 320 mm. The acquisition was split functionally into two short breath-held scans. During the first breath-hold lasting 10 heartbeats, the reference datasets for the five SA slices were acquired. Following this, a 20-heartbeat long breath-held scan was performed during which a sequence of 14 HARP (horizontally and vertically tagged) and 14 SENC (with tuning frequencies  $0.42 \text{ mm}^{-1}$  and  $0.48 \text{ mm}^{-1}$ ) images for all five slices were acquired. A tag separation of 8 mm was used for the HARP images, while a tag separation of 2.5 mm was used for the SENC images. Dense measures of Eulerian in-plane normal strain (Err and Ecc) are obtained from the HARP images by computing local spatial derivatives of the HARP phase in the appropriate directions [1]. Dense measures of Eulerian out-of-plane normal strains (Ell) are also obtained from the SENC images [2]. It can also be shown that in-plane shear strains (Ecr) and out-of-plane shear strains (Elc) can also be computed from the datasets acquired.

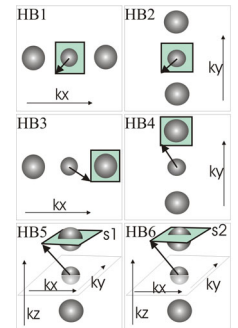


Fig. 1. A typical 6-heartbeat HARP-SENC scan

Dense measures of Eulerian in-plane normal strain (Err and Ecc) are obtained from the HARP images by computing local spatial derivatives of the HARP phase in the appropriate directions [1]. Dense measures of Eulerian out-of-plane normal strains (Ell) are also obtained from the SENC images [2]. It can also be shown that in-plane shear strains (Ecr) and out-of-plane shear strains (Elc) can also be computed from the datasets acquired.

## Results

Fig. 2 shows representative normal color-coded strain maps with in-plane synthetic tag overlay for one end-systolic time frame and an apical short-axis slice. Note the circumferential shortening, the radial thickening and the longitudinal compression in these images. In Fig. 2(c), in particular is interesting as a visual aid as in-plane synthetic tags are overlaid on an out-of-plane longitudinal strain map providing a visual correlation between in-plane motion and out-of-plane strain. To visualize strain in all five slices at once, eight regions in the left ventricle were defined and strains in each of these regions were averaged and color-coded to generate bullseye plots as seen in Fig. 3. Here, the evolution of Eulerian longitudinal strain is depicted over twelve time frames. Note the increased longitudinal shortening during end-systole.

## Discussion and Conclusion

In this paper, we have demonstrated the ability to measure the dynamic evolution of 3D myocardial strain using the HARP-SENC MRI technique. It was shown that post-processing of the datasets acquired from just two breath-holds provides full quantification and visualization of three-dimensional myocardial strain with high temporal resolution.

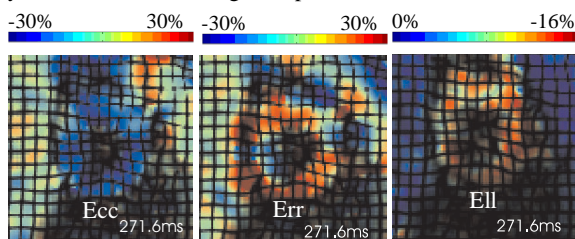


Fig. 2. Eulerian strain maps depicting (a) circumferential strain, (b) radial strain, and (c) longitudinal strain at an end-systolic time frame. In-plane synthetic tags are overlaid.

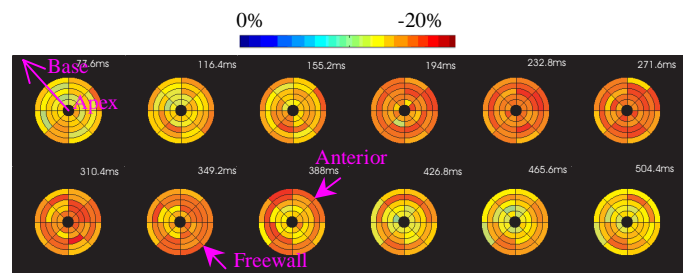


Fig. 3. Bullseye plots depicting the evolution of Eulerian longitudinal strains in octants defined in all five short axis slices.

## References

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