Quadratic Fat/Water Separation in Balanced SSFP

B. A. Hargreaves¹, D. G. Nishimura¹

¹Department of Electrical Engineering, Stanford University, Stanford, CA, United States

Introduction: Balanced steady-state free precession (SSFP) imaging suffers from bright fat signal and sensitivity to off-resonance [1,2]. Of the numerous proposed fat/water separation techniques for balanced SSFP, two are very SNR-efficient: Dixon SSFP [3] offers high image quality, but demands three or more acquisitions with varying echo times and a non-trivial reconstruction. Conversely, phase-sensitive SSFP [4] requires only one acquisition, but suffers from partial-volume effects. Neither method addresses the off-resonance sensitivity of balanced SSFP. Here we present a novel 2 point fat/water separation technique that (a) uses a simple reconstruction to separate water and fat, (b) avoids partial volume effects and (c) correctly identifies fat and water in the presence of SSFP signal nulls.

Theory: A signal S_1 with the repetition time TR and echo time TE_1 chosen such that $TR = 2TE_1 = (2n+1)/\Delta f$ (where *n* is an integer and Δf is the fat-water chemical shift) results in refocused fat and water signals with opposite sign [4]. The slowly varying phase (ϕ) can be removed robustly [5,6] leaving the real-valued water-fat difference, *d*. A second signal, S_2 , acquired at $TE_2 = TE_1 - v/(2\pi\Delta f)$ results in a phase angle v between water and fat. With $v = \pi/2$, $|S_2|^2 = W^2 + F^2 = (d - F)^2 + F^2$ (Eq. 1)

Using $|S_2|$ and *d*, the simple positive solution of (the quadratic) Eq. 1, shown graphically in Figure 1 gives the values of *W* and *F*. Although not essential for water/fat separation, the field map, *f*, can be determined (from *d*, *W*, *F*, *S*₁ and *S*₂) and used to detect pixels where crossing of an SSFP signal null has caused an incorrect sign of *d*. Negating *d* at these points, gives the accurate estimates of *W*, *F* and *f*. This is of particular significance for high-field SSFP or high-resolution SSFP, where acquisitions with and without alternating the RF phase [6,7] can be combined to remove SSFP signal nulls resulting from off-resonance.

Methods and Results: Using a 1.5T GE Excite scanner (40 mT/m gradients with 150 mT/m/ms slew rates) and a transmit/receive extremity coil, images were acquired with $TR = 2TE_I = 5.8$ ms, $TE_2 = 1.75$ ms, 30° flip angle, 160x160x64 matrix, 20x20x12.8 cm³ FOV for 3:00 scan time. A standard shim was sufficient to keep water and fat oppositely aligned in S_I . Figure 2 shows accurate fat (a) and water (b) images after phase correction of S_I and solving Eq. 1.

A second image set acquired with $TR = 2TE_1 = 13.8 \text{ ms}$, $TE_2 = 6.75 \text{ ms}$, and 30° flip angle, was repeated twice, first with RF phase alternating by 180°, then with constant RF phase [6,7] for 4 total signals. The total scan time was 15:05 for a 256x256x64 matrix over a 16x16x12.8 cm³ FOV. *W*, *F* and *f* were calculated as above for both phase cycles. At points where *f* deviated by more than an empirically determined threshold of 140 Hz, *d* was negated and *W* and *F* were recalculated. Finally, at each pixel, the maximum [7] from the two phase cycles was taken for both *W* and *F* images, which are shown in Figure 3.

Discussion: We have presented a quadratic water/fat separation technique for balanced SSFP that is simpler and requires fewer acquisitions than recent Dixon methods, while eliminating the partial-volume effects of phase-sensitive SSFP. This method is similar to that shown by Xiang [8], but also exploits the refocusing effect of balanced SSFP. The value of v can be any non-zero angle, but will, along with fat/water fraction, affect the propagation of noise. Extending TR minimizes efficiency loss from use of multiple echo times, and the multiple-phase-cycle approach here enables accurate fat/water separation for high-field or high-resolution SSFP in reasonable scan times.

References:

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Figure 1. Geometric interpretation of Eq. 1: The (W,F) content is the intersection in W-F space of a line of slope 1 and W-intercept d, with a circle of radius $|S_2|$.



Figure 2. Sagittal knee images of separated fat (a) and water (b) components for TR=2TE=5.6 ms.



Figure 3. Sagittal knee images for TR=2TE=13.8 ms. Source S_2 images (a) and (b) with alternating and non-alternating RF phase have null-signal areas (arrows). Water (c) and fat (d) images after maximum-combination of separated images for each RF phase scheme.