

Comparison Between Hahn Spin Echo and Gradient Echo Sampling of the Spin Echo (GESSE) T₂ Measurements at Ultra-High Field Strength

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Introduction: Knowledge of T₂ relaxation times at ultra-high field strength (≥ 7 T) is needed for optimizing acquisition parameters for T₂-weighted imaging and understanding relaxation mechanisms. However, standard T₂ measurements (e.g., using Hahn or Carr-Purcell-Meiboom-Gill Spin Echo (SE)) at ultra-high field strength are affected by severe radiofrequency (RF) magnetic field (B₁) inhomogeneity [1], which results in substantial variations of the flip angle and receive sensitivity across the field-of-view (FOV) [2]. Such T₂ measurements at 8 T were found to be accurate only in regions where the flip angle remains within ±20° from 90° [3]. The Gradient Echo Sampling of the Spin Echo (GESSE) T₂ measurement method was shown to be less sensitive to B₁ inhomogeneity at 1.5 T [4]. We implemented this method at ultra-high field strength and compared it with Hahn SE T₂ measurements in a phantom as well as *in vivo* and postmortem human brains. The B₁ inhomogeneity was also experimentally mapped to assess the B₁ sensitivity of both methods.

Methods: The studies were performed on an ultra-high field human whole-body MRI system using transverse electromagnetic RF head coils. Due to the flip angle variability, we first defined a “nominal” flip angle (FA) as the average flip angle in a 1 cm³ region of interest (located in the hippocampus for human studies), determined the transmit power level resulting in a nominal FA of 90° using a voxel-selective stimulated echo sequence, and then used this reference to set the transmit power level corresponding to a chosen nominal FA. Four Hahn SE images were acquired with different TEs and a T₂ map computed by fitting a monoexponential decay pixel-by-pixel. For the GESSE method, a SE image was acquired at TE and two asymmetric SE images at TE ± ΔTE using readout gradients of same polarity to avoid misregistration errors due to gradient imperfections. A T₂ map was then computed as $T_2 = 2 \Delta TE / \ln[S(TE - \Delta TE) / S(TE + \Delta TE)]$ [4]. Preliminary studies confirmed that the error is minimal when TE ~ T₂ and ΔTE > T₂/4. To quantify the B₁ inhomogeneity, maps of the local flip angle α and receive sensitivity r were experimentally measured from two series of gradient echo images acquired with TR ≫ T₁ and nominal FA α₀ and 2α₀. A flip angle map was computed as $\alpha = \cos^{-1}(S_{2\alpha} / 2S_{\alpha})$ [5], then a map of ρ r was computed as $S_{\alpha} / \sin(\alpha)$ and low pass filtered to yield a measure of the receive sensitivity.

To quantify the sensitivity of the T₂ measurements to B₁ inhomogeneity, we studied a 1.5 L phantom (4% agarose, 2 mM CuSO₄, 0.125 M NaCl, T₁ = 630 ms) using TR 3000 ms, TE 20/40/70/110 ms (Hahn SE) or TE/ΔTE 40/10 ms (GESSE), nominal FA 90°/180°, FOV (18 cm)², matrix (MTX) 256x128, one 3 mm thick slice for the T₂ measurements, and TE 7 ms, MTX 128x64, nominal FA 60°/120°, and otherwise identical parameters for the B₁ mapping. We also studied 5 healthy volunteers (2 male, 3 female, age 20–49) who gave informed consent and 5 postmortem unembalmed human subjects (2 male, 3 female, age 57–85). Typical parameters were TR 1500 ms, TE 20/50/90/135 ms (Hahn SE) or TE/ΔTE 50/13 ms (GESSE), nominal FA 90°/180°, FOV (16 cm)², MTX 512x256, one 3 mm thick slice for the T₂ measurements, and TR/TE 4000/7 ms, nominal FA 60°/120°, MTX 256x64, and otherwise identical parameters for the B₁ mapping.

Results: Figure 1 shows the results of the phantom study. The GESSE T₂ map is more homogeneous than the Hahn SE T₂ map and the GESSE T₂s are generally lower than the Hahn SE T₂s. The banding artifacts in the GESSE T₂ map can be attributed to shim/gradient instability. As expected, there are substantial variations of the flip angle and receive sensitivity. The Hahn SE T₂s tend to increase as the flip angle deviates from 90°, whereas the GESSE T₂s are independent of the flip angle. Both Hahn SE and GESSE T₂ measurements become noisier as the flip angle decreases. The average Hahn SE T₂ at a flip angle of 90° is higher than the average GESSE T₂.

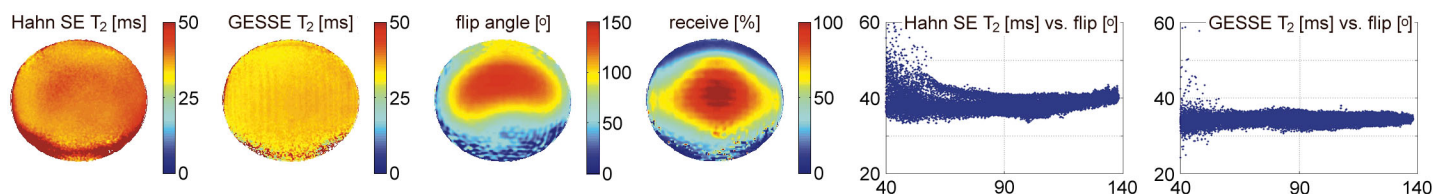


Figure 1: Results of the phantom study. On both plots, pixels with a receive sensitivity lower than 25% and therefore excessive noise were excluded.

Figure 2 shows the results of an *in vivo* study. In the central region where flip angles are much larger than 90°/180°, Hahn SE T₂s are very high, as in the phantom. In the lateral parts of the temporal lobes where the flip angles and/or receive sensitivity are low, both Hahn SE and GESSE methods become inaccurate and Hahn SE T₂s are again very high. On the other hand, in regions where flip angles are close to 90°/180°, both methods provide similar results, with GESSE T₂s somewhat lower than Hahn SE T₂s, as in the phantom. Furthermore, the GESSE T₂ map clearly shows some nuclei with lower T₂s (arrows), which are not seen on the Hahn SE T₂ map. As for the phantom, banding artifacts in the GESSE T₂ map can be attributed to system instability.

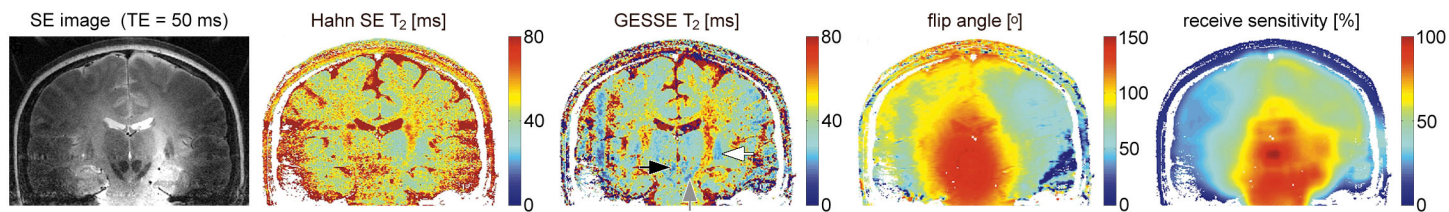


Figure 2: Results of an *in vivo* study (29-year-old female). Black arrow = red nucleus, gray arrow = substantia nigra, white arrow = globus pallidus.

Discussion: The GESSE method offers significant advantages over the Hahn SE method. First, it requires a substantially shorter scan time (25% in our case) and is thus more suitable for *in vivo* studies. Second, it is less sensitive to B₁ inhomogeneity, which is severe at ultra-high field strength. Furthermore, one reason why Hahn SE T₂s are higher than GESSE T₂s may be that the Hahn SE signal decay is not simply monoexponential but depends on water diffusion in magnetic field gradients [6], especially in the nuclei. The GESSE method is by design not affected by this effect [4], and therefore provides more accurate T₂ measurements. On the other hand, GESSE T₂ maps are noisier than Hahn SE T₂ maps. This is because the former are computed from only two images, whereas the latter are computed from four. The short T₂s at ultra-high field strength limit the TE and therefore the number of echoes that can be acquired. In addition, the GESSE T₂ maps are computed from a ratio of images, which is more sensitive to error propagation than the exponential fit used to compute the Hahn SE T₂ maps.

Conclusion: The GESSE method is significantly faster, less sensitive to B₁ inhomogeneity, and more accurate than the Hahn SE method, thus making it clearly preferable for T₂ measurements at ultra-high field strength, despite the lower signal-to-noise ratio.

References [1] Majumdar S. *MRM* 1986;3:397. Crawley AP. *MRM* 1987;4:34. Poon CS. *JMRI* 1992;2:541. Sled JG. *MRM* 2000;43:589 [2] Ibrahim TS. *Phys Med Biol* 2001;46:2545 [3] Whitaker CDS. *ISMRM* 2003. p. 1098 [4] Yablonskiy DA. *MRM* 1997;37:872 [5] Insko EK. *JMR A* 1993;104:78 [6] Carr HY. *Phys Rev* 1954;94:630