

Alignment of Ventilation and Perfusion Images at Acquisition: Validation in a Porcine Model

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Introduction: Quantitative and comprehensive assessment of lung function has proven to be very demanding in that it requires regional information about both alveolar V and Q. One of several recently developed noninvasive methods for MR imaging of V [1] utilizes exogenous airway contrast agents such as hyperpolarized (HP) ³He. Similarly, one method used to obtain quantitative images of Q is that of a dynamic gadolinium study [3]. Though previously shown applicable to several physiological conditions, the methods show difficulty in calculating regional V/Q because simultaneous values for each parameter of lung function are required. Furthermore, regional V/Q computation requires spatial matching of V and Q images, and to our knowledge no validation method has been reported on registration of lung MR V/Q images even when acquired in a controlled situation. In this work, we use a post image processing technique to quantify the degree of misregistration between MR V/Q images at the time of acquisition and confirm that it is possible to acquire data that are co-registered within an acceptable range of a few degrees in rotation and a fraction of a millimeter in translation.

Methods: Experiments were conducted on 25-35 kg Yorkshire pigs (N=5) under ketamine/isoflurane anesthesia. The pigs were ventilated and transferred supine to a 1.5T imaging system configured for broadband acquisition and double tuned bird-cage coil used for signal reception was double tuned to ³He and proton frequencies. V and Q images were obtained using HP ³He and gadolinium, respectively, as was described in [1, 2]. Absolute translations and rotations around different axes needed to register the images were computed as a measure of initial misregistration. Because V and Q images were acquired with the same amount of gas inhalation, the task was considered to be a rigid body registration. The mutual information (MI) based method of rigid body registration has been proven superior when intensity characteristics are dissimilar [4]. The method maximizes the information that one volumetric image provides about the other and seeks for an optimum transformation T that registers the reference image C₁ with the test image C₂ by maximizing their mutual information as follows:

$$T = \max_T I(C_1, T(C_2)), \quad (1)$$

where, $I(C_1, T(C_2)) = h(C_1) + h(T(C_2)) - h(C_1, T(C_2)) \quad (2)$

In (2), $h(\cdot)$ is the entropy of the histogram of an image and $h(\cdot, \cdot)$ is the entropy of the joint histogram of two images. For each pair of images rotational and translational components of T were computed to quantify the initial misregistration.

Figure 1:

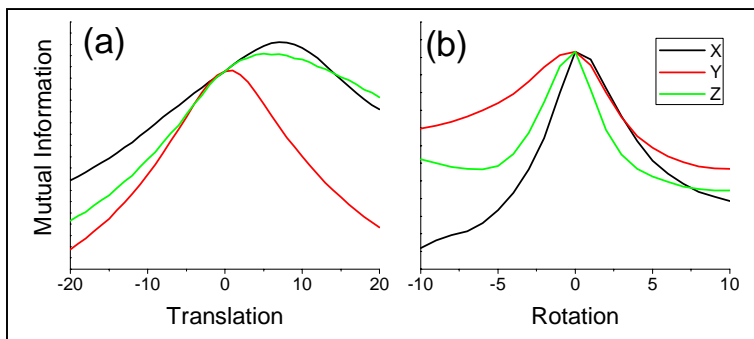


Table 1	Mean	Std Dev
Trn. x-axis	5.6 mm	5.3 mm
Trn. y-axis	2.6 mm	0.68 mm
Trn. z-axis	6.8 mm	7.2 mm
Rotation x	0.34°	0.17°
Rotation y	0.31°	0.25°
Rotation z	0.17°	0.19°

Figure 2:

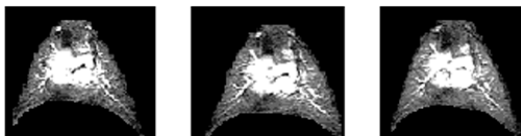


Figure 3:



Results and Discussion: Means and standard deviations for the 5 studies in terms of absolute translation and rotation around three axes are shown in Table 1. Figures 1A and B are two partial plots of MI values for translation and rotation around each of the three axes, respectively. Figures 2 and 3 illustrate 2-D gradient-echo images, one (3) of which shows ³He distribution obtained in one pig, suggesting normal V, while the other (2) shows the Q image of the same subject. Though limitations of co-registration technology range from physiological variations to co-registration characteristics, the results of our preliminary study demonstrate that, under a controlled situation and proper imaging protocol, it is possible to achieve approximately co-registered images of V and Q (within 1-2 voxels of perfect alignment). This preliminary work is crucial because it allows reliable quantitative measurements of regional V and Q to be obtained in both normal and diseased lungs. In this manner 'responders' versus 'nonresponders' to clinical therapies could be identified, and the lung's subsequent response to acute therapy could be monitored.

Acknowledgments: This work was supported by NIH grants RO1-HL64741A and performed at the MMRRCC, a NIH supported resource center (RR02305).

References: 1. de Lange EE, et al. Radiology 1992;210:851-857. 2. Kauczor HU. NMR in Biomedicine 2000;13:173-5. 3. Hatabu H, et al. Magn Reson Med 1996;36:503-508. 4. Hagemann A RK, et al. Medical Image 1999;18:875-884.