

The influence of membrane permeability on bi-exponential behavior of diffusion-attenuated MR signal from a single cell

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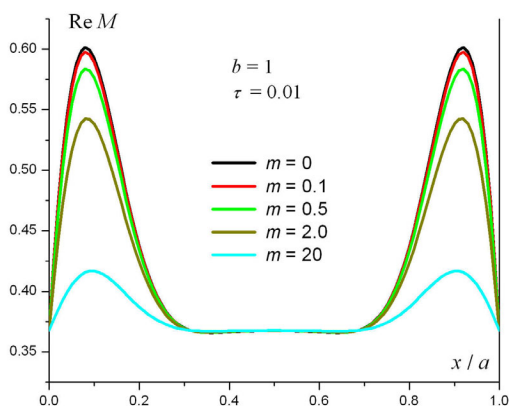
We recently analyzed in detail the behavior of the diffusion-attenuated MR signal in a single compartment with impermeable boundary (1). It was shown that for short diffusion time $\Delta = t_D$, $t_D = a^2 / D$ is the characteristic diffusion time (a is a compartment size, D is the free-diffusion coefficient), the signal dependence on the b -value can be approximated to a remarkable degree by the bi-exponential function $S^0 = f_1 \exp(-bD_1) + (1 - f_1) \exp(-bD_2)$. The physical underpinning of this approximation is the presence of a strongly inhomogeneous distribution of magnetization at $\Delta = t_D$. Here all spins can be conditionally divided into two populations: one population, comprising spins located far from the boundary, can be considered as unrestricted (fast-diffusing pool); the other population, comprising spins located near the boundary, is restricted due to encounters with the boundary (slow-diffusing pool). The subject of this communication concerns the manner in which a boundary with finite permeability μ “nibbles” at the slow-diffusing pool and affects the bi-exponential behavior of the signal.

For short diffusion times, the MR signal from a single compartment of a size a is similar to the signal from a one-dimensional periodic structure of period a , which allows an exact analytical solution. In the narrow pulse approximation, we find rather simple expressions for the local magnetization distribution inside the compartment $M(x, \Delta)$ and the net spin echo signal $S(\Delta)$:

$$M(x, \Delta) = \sum_n \frac{2iq \exp(-iqx) \cdot \exp(-\kappa_n^2 \tau) \kappa_n [\cos(\kappa_n(1-x/a)) - \exp(iq) \cos(\kappa_n x/a)]}{((qa)^2 - \kappa_n^2) (2m+1) \sin \kappa_n + \kappa_n \cos \kappa_n}, \quad [1]$$

$$S(\Delta) = \frac{2q^2}{m} \sum_n \frac{\exp(-\kappa_n^2 \tau) \kappa_n^2}{((qa)^2 - \kappa_n^2)^2 (2m+1 + \kappa_n \cot \kappa_n)} \quad [2]$$

where $q = \gamma G \delta$, γ is the gyromagnetic ratio, G is a field gradient, δ is a pulse duration, $\tau = \Delta / t_D$, $m = \mu a / D$, κ_n are non-negative roots of the equation $2m(\cos \kappa - \cos(qa)) = \kappa \cdot \sin \kappa$. In the limit of completely permeable membranes (free diffusion, $m = \infty$), Eq. [1] reduces to the standard homogeneous magnetization $M(x, \Delta) = \exp(-Dq^2 \Delta)$. In the opposite limit of completely impermeable membranes, Eq. [2] reduces to the well-known result (2).



As an example, the real part of the function $M(x, \Delta)$ is shown in Fig. 1 for several values of the dimensionless permeability m (time Δ and the b -value $b = (qa)^2 \Delta$ are fixed as indicated). Note that for $m \leq 0.1$ the magnetization distribution practically coincides with the case of a completely impermeable boundary. The two clearly distinguished maxima in M , making up the slow-diffusing pool, decrease as m increases and it should be expected that the apparent volume fraction of this pool f_1 also must decrease. Modeling the net signal $S(\Delta)$ as a bi-exponential function shows that as m increases f_1 decreases from $\sim 10\%$ at $m=0$, to 8% at $m=1$ (typical of mammalian cells), to 1% at $m=20$, the apparent diffusion coefficient D_2 of the fast-diffusing pool approaching D , and D_1 tending to $0.44 D$.

We conclude that bi-exponential signal behavior predicted at short diffusion time $\Delta = t_D$ for a single compartment with impermeable boundary [1] is still found in the presence of a boundary with finite permeability in the range expected of biological membranes.

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