

A 3D PR Sequence (PR-TRICKS) for Dynamic Contrast Enhanced (DCE) Imaging of the Breast

S. B. Fain¹, J. Du¹, R. Parakkal², C. Moran¹, F. Kelcz³, T. Carroll⁴

¹Medical Physics, University of Wisconsin, Madison, WI, United States, ²Biomedical Engineering, University of Wisconsin, Madison, WI, United States, ³Radiology, University of Wisconsin, Madison, WI, United States, ⁴Biomedical Engineering, Northwestern University, Chicago, IL, United States

INTRODUCTION

Breast MRI has been shown to have high sensitivity but variable specificity for the detection of breast cancer [1,2]. The temporal analysis of dynamic contrast enhanced images has shown promise as method to characterize benign and malignant lesions in breast MRI [3]. While high spatial resolution is needed to localize lesions using DCE-MRI, high temporal resolution is also needed to more accurately depict the contrast uptake or “wash in” by the tumor [4]. Several non-Cartesian MRI acquisition sequences have been proposed to improve the spatial and temporal resolution of DCE breast MRI including spiral [5] and projection acquisition [6] methods. The PR-TRICKS method, which uses undersampled projection acquisition (PR) in-plane and TRICKS [7] in the slice direction, has been shown to demonstrate contrast uptake dynamics in MR angiographic applications [8]. The purpose of this work is to apply a modified version of the PR-TRICKS acquisition to perform DCE-MRI of the breast at high temporal and spatial resolution to improve the characterization of breast lesions.

MATERIALS AND METHODS

The modified version of the PR-TRICKS sequence consists of 3 phases: A mask phase in which all projection angles and all Fourier views are acquired, a dynamic phase during contrast wash-in which all projection angles are acquired but only the center-most k-space views are acquired every 4-7 s, and a washout phase in which the volume was acquired at full resolution every 8-14 s (Fig.1a). Projection angles are dithered to so that under-sampling is reduced for larger temporal apertures.

Phantom and volunteer experiments were performed on a 1.5 T scanner (Signa LX; GE Medical Systems, Milwaukee, WI) using a commercial breast coil (Medical Advances, Milwaukee WI) and an rf-spoiled GRE pulse sequence. Common parameters for these experiments: azimuthal sampling 36-72 projections, ± 64 kHz bandwidth, and 15° flip. Specific to the phantom experiments a $256 \times 256 \times 36$ matrix was used with a 30 cm FOV yielding a $1.2 \times 1.2 \times 2.2$ mm³ voxel size and a TR/TE 5.3/1.1 ms. A spatial resolution phantom was combined with a flow phantom (Fig. 1b-d) to demonstrate the ability to measure contrast wash-in and out while maintaining spatial resolution. The temporal resolution of the PR-TRICKS was varied from 4-7 s during the wash-in phase and 8-12 sec during contrast wash-out. A reference curve was measured independently using a 2D GRE sequence with a 0.4 s resolution. In the volunteer studies Gadodiamide (Omniscan, Amersham Health, Princeton NJ) was injected intravenously (0.1 mmol/kg) at 3 cc/s. For the volunteer with bilateral lesions, a bilateral DCE-MRI data set was acquired using the modified PR-TRICKS at a FOV of 28 cm, $384 \times 384 \times 48$ matrix, for a $0.7 \times 0.7 \times 2.2$ mm³ voxel size, TR/TE 6.9/1.2 ms. The temporal resolution for the wash-in phase was 6 s and for wash-out was 14 s.

RESULTS and DISCUSSION

The contrast uptake was accurately measured for both PR-TRICKS time resolutions although the wash out lagged as expected (Fig 1a). In plane resolution of 1.2 mm was maintained throughout (Fig 1d). The slice resolution varied from approximately 5 mm during the wash-in to 2.2 mm during the wash-out (Fig 2 a and b). Both the tumors were detected using the 3D PR-TRICKS. The rim-enhancing tumor in the right breast (Fig.3a, upper arrow) was diagnosed as malignant based on permeability $>1.2 \text{ min}^{-1}$ while the smaller fibroadenoma in the left breast (lower arrow) was misdiagnosed as malignant due to an early intense wash-in at 24 s post-injection, perhaps due to first-pass vascular volume. The second volunteer did not receive contrast but the in-plane resolution is demonstrated for a unilateral sagittal study (Fig 3b).

CONCLUSIONS

We have shown the feasibility for breast MR using 3D PR-TRICKS for DCE-MRI of Breast. We are currently conducting a pilot study in 10 patient volunteers with known masses to assess the performance of this technique in a non-blinded study. Subsequent to this, the method will be applied to a larger patient study of 70 volunteers to assess in a blinded fashion the performance of the sequence for characterizing breast lesions in a clinical setting.

REFERENCES: 1. Kuhl, C.K et al., *Radiology* 211:101-110, 1999.; 2. Kinkel, K. et al., *Seminars in Surgical Oncology* 20:187-196, 2001.; 3. Evelhoch, J.L., *JMRI* 10:254-259, 1999.; 4. Henderson E. et al., *Magn. Reson. Imaging* 16:1057-1073, 1998.; 5. Yen, YF, et al., *Magn. Reson. Med.*, **11**, 351, 2000.; 6. Song, HK, et al., *Magn. Reson. Med.*, **46**, 503, 2001.; 7. Korosec et al. *MRM*, 36:345-351, (1996). 8. Vigen, KK, et al., *Magn. Reson. Med.*, **43**, 170, 2000. **The authors acknowledge the Komen Foundation.**

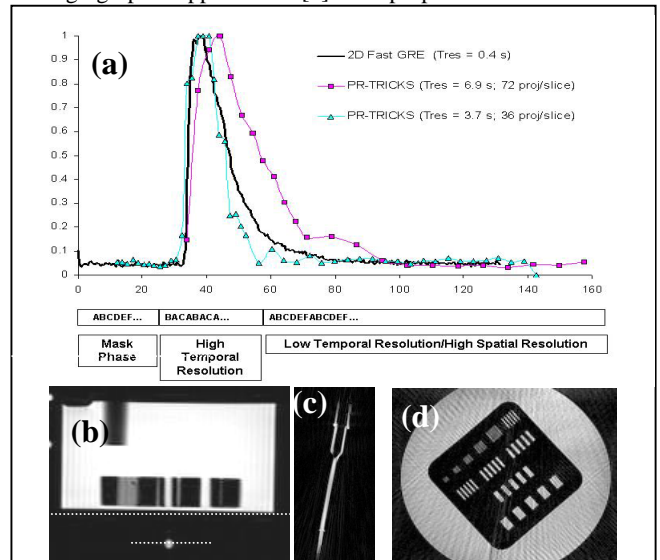


Figure 1: (a) Phantom experiment time courses measured using modified 3D PR-TRICKS. (b) phantom design showing carotid flow and resolution phantom in axial plane. (c) Carotid flow phantom and (d) resolution phantom showing in-plane resolution.

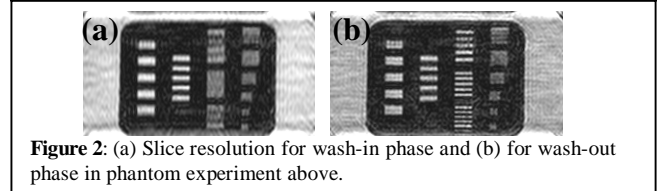


Figure 2: (a) Slice resolution for wash-in phase and (b) for wash-out phase in phantom experiment above.

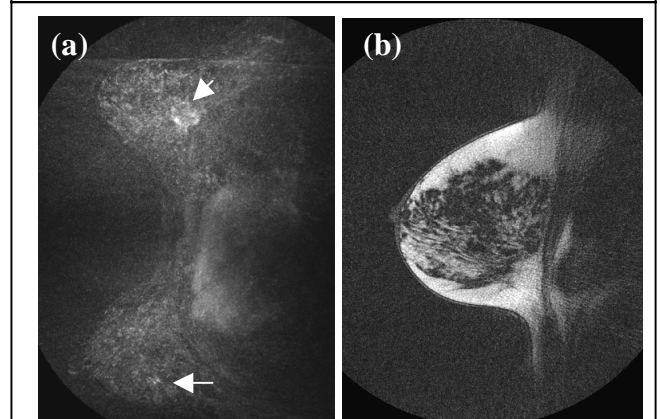


Figure 3: (a) PR-TRICKS 0.7 x 0.7 mm in-plane resolution. Malignant lesion in right breast (upper arrow) and benign in left breast (lower arrow). (b) Central slice from sagittal unilateral study.