

T₂ Relaxation Study of Water in Human Brain using Carr-Purcell Spin-Echoes at 4T and 7T. Frequency shift Δω at 4T and 7T.

S. Michaeli¹, K. Ugurbil¹, M. Garwood¹

¹Center for Magnetic Resonance Research, University of Minnesota School of Medicine, Minneapolis, MN, United States

Synopsis Fully adiabatic Carr-Purcell (CP) type sequence (CP-LASER) with SPIRAL readout was used to investigate the change in Δω (difference in angular Larmor frequency) with the field (4T vs. 7T). High resolution T₂ – weighted images were acquired to measure the apparent T₂[†] in human visual cortex V1 as a function of interpulse time interval in CP train. It was found that Δω increases slightly with the field but significantly less than linearly. This suggest that chemical exchange does not explain the data and that Nuclear Overhauser Effect (NOE) and/or NOE in the rotating frame (ROE) are contributing to MR signal decay.

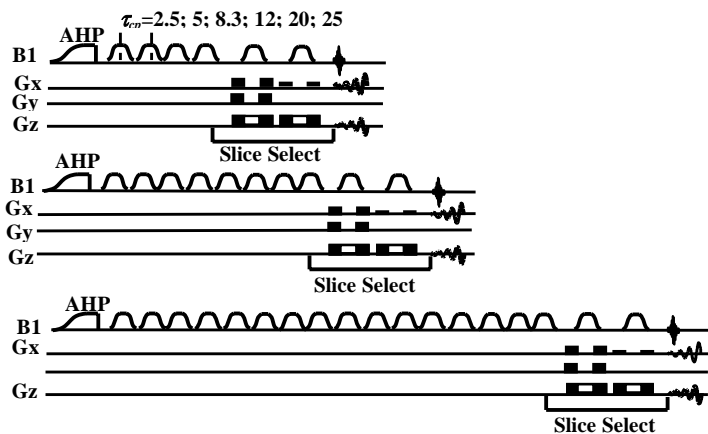
Introduction

In iron-rich regions of the brain the proton MR transverse relaxation rates measured with a CP sequence has been observed to depend significantly on the interpulse time interval (τ_{cp}). It was suggested that this effect is important for in-vivo quantification of brain iron, because of its relevance to several neurodegenerative disorders, including Parkinson's and Alzheimer's diseases as well as for the understanding of the mechanisms of Blood Oxygenation Level Dependent (BOLD) contrast. General theory was presented recently^{1,2} for weakly magnetized particles and applied to randomly distributed spheres. In this theory, the Luz-Meiboom Chemical Exchange (CE) model was compared with the theories of T₂-shortening caused by microscopic magnetic centers, namely: inner- and outer sphere relaxation theories in the long-echo limit and mean gradient diffusion theory for the short-echo limit. It was demonstrated, that at the short – echo limit, when τ_{cp} << τ_d (τ_d is the diffusion correlation time), the classical theory of diffusion in magnetic gradients derived originally by Carr and Purcell, may be used. In the long echo limit (τ_{cp} >> τ_d), the standard relaxation theory applies and no T₂[†] dependence on τ_{cp} was predicted. Generally, those theories predict a square dependence of the relaxation rate on the Δω: [1/T₂]_{CE} ~ F_aF_b (Δω)²τ_{cp}² / τ_d (τ_{ex}); (τ_{cp} << τ_d (τ_{ex})). At the long-echo limit: [1/T₂]_{CE} ~ F_aF_bτ_{ex}(Δω)²; (τ_{cp} >> τ_{ex}), where the F_a and F_b = fraction of protons in each site (F_a+F_b=1), τ_a and τ_b – residence times in each site, Δω- difference in angular Larmor frequency at site b relative to site a. The relaxation rates are described by equation (1):

1/T₂[†] = 1/T₂ⁱⁿ + Δω²τ_{cp} αβx {1-b x tanh [1/(bx)]}; x=τ_d/τ_{cp}; τ_d=r²/D, where D is apparent diffusion coefficient, τ_d-diffusion time. The intrinsic relaxation rate is defined as: 1/T₂ⁱⁿ=1/T₂^{DD} + σ, where the first and second terms spin dipolar interactions and the dipolar cross-relaxation, respectively. The goal of this study was to measure intrinsic transverse relaxation times at 4T and 7T in human brain visual cortex V1 and to investigate Δω at 7T comparatively to 4T. These results provide important information on the contribution of dynamic dephasing to the MR signal decay and suggest another mechanisms, namely nuclear Overhauser effect (NOE) and/or the rotating-frame-NOE (ROE), that are operative in the sample.

Methods

1D CP-LASER-SPIRAL



Imaging studies were conducted with 4T and 7T whole body MRI/MRS systems. A ¹H quadrature surface coils consisting of two geometrically decoupled turns (each 7 cm in diameter) were used for the measurements at 4T and 7T. High resolution T₂ – weighted images (0.7 x 0.7 mm² in-plane resolution) were acquired to measure the apparent T₂[†] with CP-LASER³ sequence with SPIRAL readout.⁴ In CP-LASER, (Fig. 1) the length of CP-train was increased by inserting additional AFP pulses between the excitation pulse and the two AFP pulses used for slice selection. T₂[†] values were measured with different interpulse time intervals in the CP train: τ_{cp} = 2.5, 5, 8.3, 12, 20, 25 ms. TR=4s/segment was used to minimize T₁ contribution. For slice selection and in CP-train HS1-R10 adiabatic pulses were used. Images were recorded using: FOV = 18 cm, 256-matrix and 8 segments, at = 35 ms, thickness 4 mm. Slice-selection and the SPIRAL portions of the sequence were kept constant for all acquisitions, thus the T₂^{*} weighting introduced by this portion was constant.

Fig.1 Schematic representation of the CP-LASER sequences with SPIRAL readout.

Results and Discussion

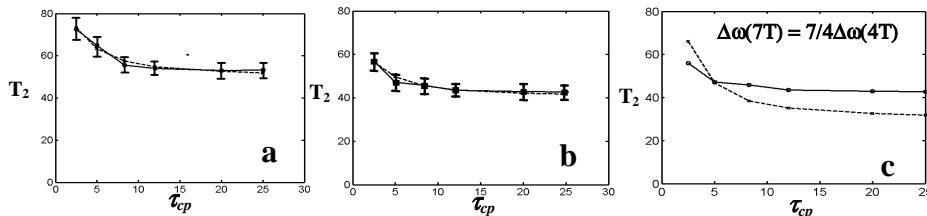


Fig.2 Averaged calculated T₂[†] time constants at 4T ((a), 6 individuals) and at 7T ((b), 5 individuals) as a function of τ_{cp} and the theoretical simulations using Eqn. (1) (dashed line). c) theoretical simulation using ratio Δω(7T)=7/4Δω(4T), superimposed on 7T experimental results.

Schematic representation of the CP-LASER sequence used for the T₂[†] measurements is shown on Fig. 1. Fig.2 demonstrates the T₂[†] dependence on τ_{cp}. At short τ_{cp} a squared dependence of T₂[†] on τ_{cp} was observed, while at long τ_{cp} the T₂[†] were independent on τ_{cp}. As expected, the T₂[†] measured at 7T were shorter than at 4T (significant difference; p<0.001, two-tailed). From the theoretical simulations the best fit to the experimental data was found with τ_d = 11 ms at both 4T and 7T, Δω (7T) ~ 1.1 Δω(4T) and T₂ⁱⁿ = 83 ms at 4T and T₂ⁱⁿ = 63 ms at 7T. The following features of the simulation results should be pointed out: (i) shortening of T₂ⁱⁿ from 4T to 7T; (ii) lack of the linear field dependence of Δω at 7T comparatively to 4T. A possible explanation of increase of the apparent transverse relaxation rate with the field is the dipolar cross-relaxation of through-space interacting spins. The deviation of the Δω increase from 4T to 7T from linearity suggests a contribution of a mechanism other than the chemical exchange on τ_{cp} dependence of the transverse relaxation rate, namely: dipole-dipole interaction of the coupled spin packets, that lead to polarization/coherence transfer detected with CP-LASER technique.

References

1. R. Brooks, et al., MRM 45, 1014-1029 (2001); 2. J. Jensen et al., MRM 46: 159-165 (2001); 3. Garwood, M. et al., JMR 153: 155-177, 2001; 4. Pfeuffer J. et al., MRM 47: 344-353 (2002).

Acknowledgment This research was supported by NIH grants P41 RR08079, NS38070 and NS39043, Keck Foundation and National Foundation for Functional Brain Imaging and the US Department of Energy.